

Fundamentals of Microscopy Course Light Properties and Optical Principles

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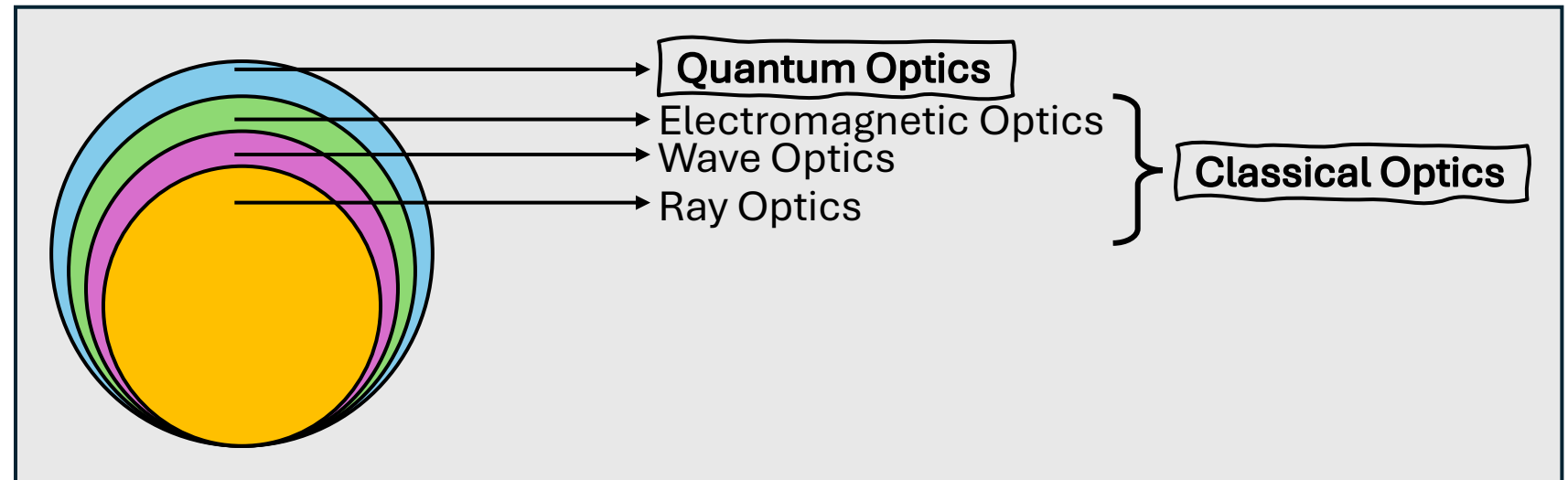
The Rockefeller University

Outline

- Definitions
- Electromagnetic fields and spectrum
- EM field propagation (reflection, refraction)
- EM field interference and diffraction
- Manipulation of light rays
- Building a basic microscope
- Imaging, resolution, numerical aperture

Definition

- **Optics:** branch of Physics that studies the behavior and properties of light, its generation, propagation, interaction with matter, and detection.
- **Light:** electromagnetic radiation that can be detected by the human eye; shows both wave and particle characteristics (visible EM).
- **Photon:** the smallest **discrete** amount or quantum of electromagnetic radiation; has zero (rest) mass and travels at $c = 299,792,458$ m/s.



Photonics: science and technology of generating, controlling, and detecting photons (i.e., “particles” of light).

Biophotonics: optics with an emphasis on **interaction** of light with **biological** tissues

Biomedical Optics: design and application of advanced optical techniques to solve problems in **medicine** and **biology**

Basis of geometrical optics

Rectilinear propagation of light rays

Law of reflection,

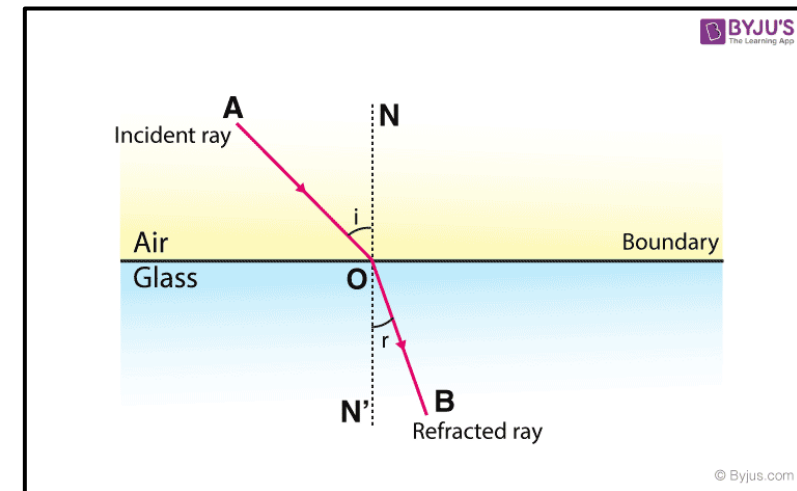
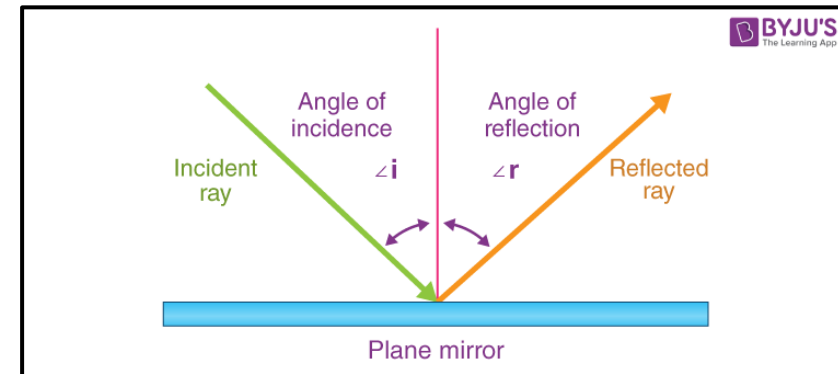
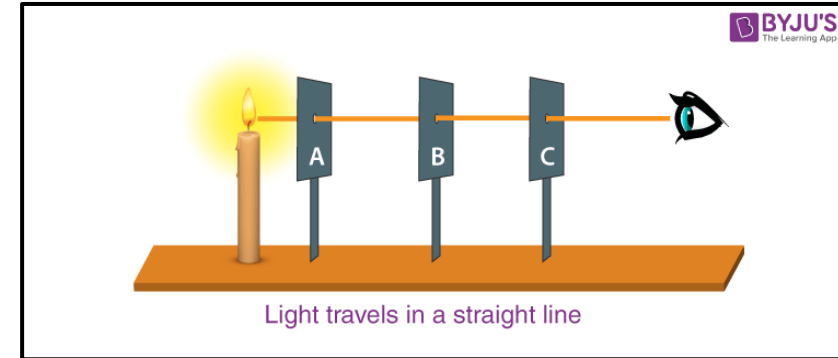
(Euclid ~ 300 BC)

shortest path,

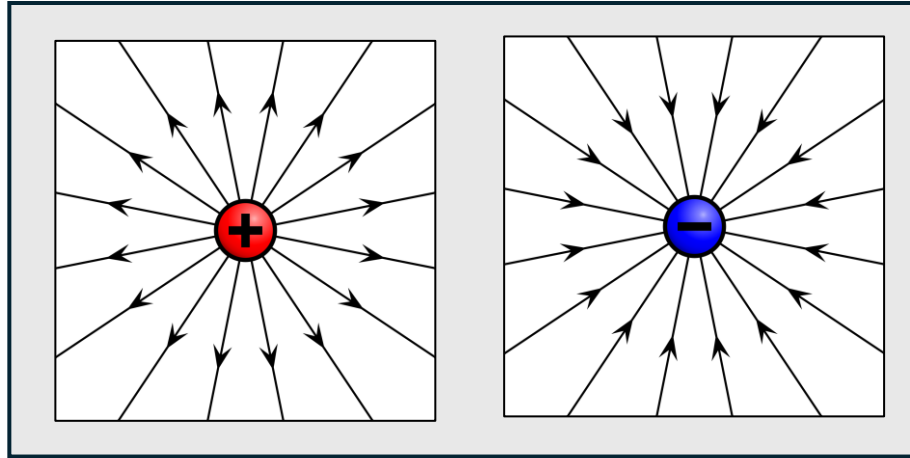
(Hero's principle ~100 A.D.)

law of refraction,

dates to Ptolemy (~170 A.D.)

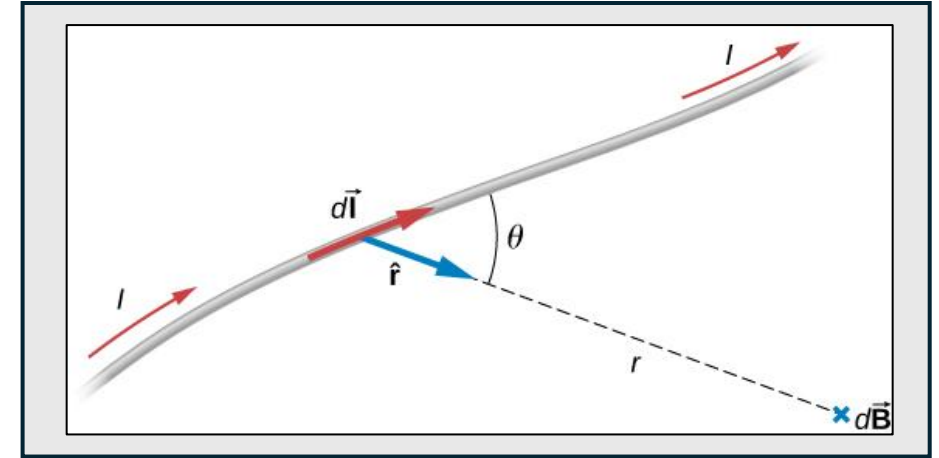


Electric and magnetic fields



$$\vec{E}_q = \frac{1}{4\pi\epsilon_0} \left(\frac{q}{r^2} \hat{r} \right)$$

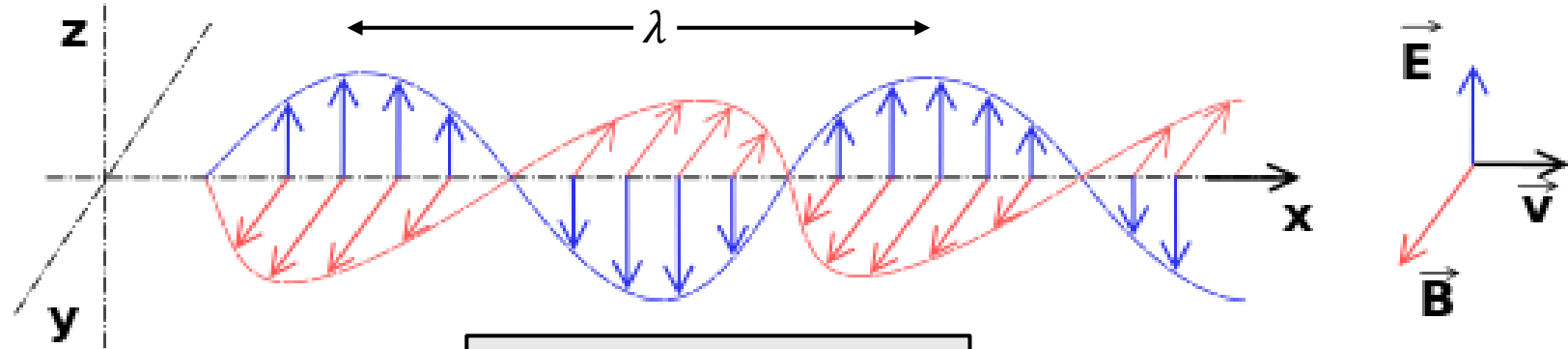
Electric field
stationary electric charge q ,
at distance r
in vacuum (ϵ_0)
 $\epsilon_0 = 8.854187 \times 10^{-12} \text{ F m}^{-1}$
(vacuum electric permittivity)



$$\vec{B} = \frac{\mu_0}{4\pi} \int_{\text{wire}} \frac{I d\vec{l} \times \hat{r}}{r^2}$$

Magnetic field
wire carrying current I ,
at position r
in vacuum (μ_0)
 $\mu_0 = 4\pi \times 10^{-7} \text{ H/m}$
(vacuum magnetic permeability)

Electromagnetic fields



$$c = f\lambda \text{ (in vacuum)}$$

$$E = hf = h\frac{c}{\lambda}$$

$$c = 299,792,458 \text{ m/s}$$

Vector Wave Equation
(second-order linear PDE)

$$\nabla^2 \vec{E} = \mu_0 \epsilon_0 \frac{\partial^2 \vec{E}}{\partial t^2}$$

$$c = \frac{1}{\sqrt{\epsilon_0 \mu_0}} = 3 \times 10^8 \left(\frac{m}{s}\right) \text{ speed of light in vacuum}$$

$$v = \frac{1}{\sqrt{\epsilon \mu}} \text{ speed of light in medium}$$

$$n = \frac{c}{v} = \sqrt{\frac{\mu \epsilon}{\mu_0 \epsilon_0}} \text{ refractive index}$$

Maxwell's differential equations (in vacuum)
(linear, first-order partial differential equations (PDEs) in terms of field)

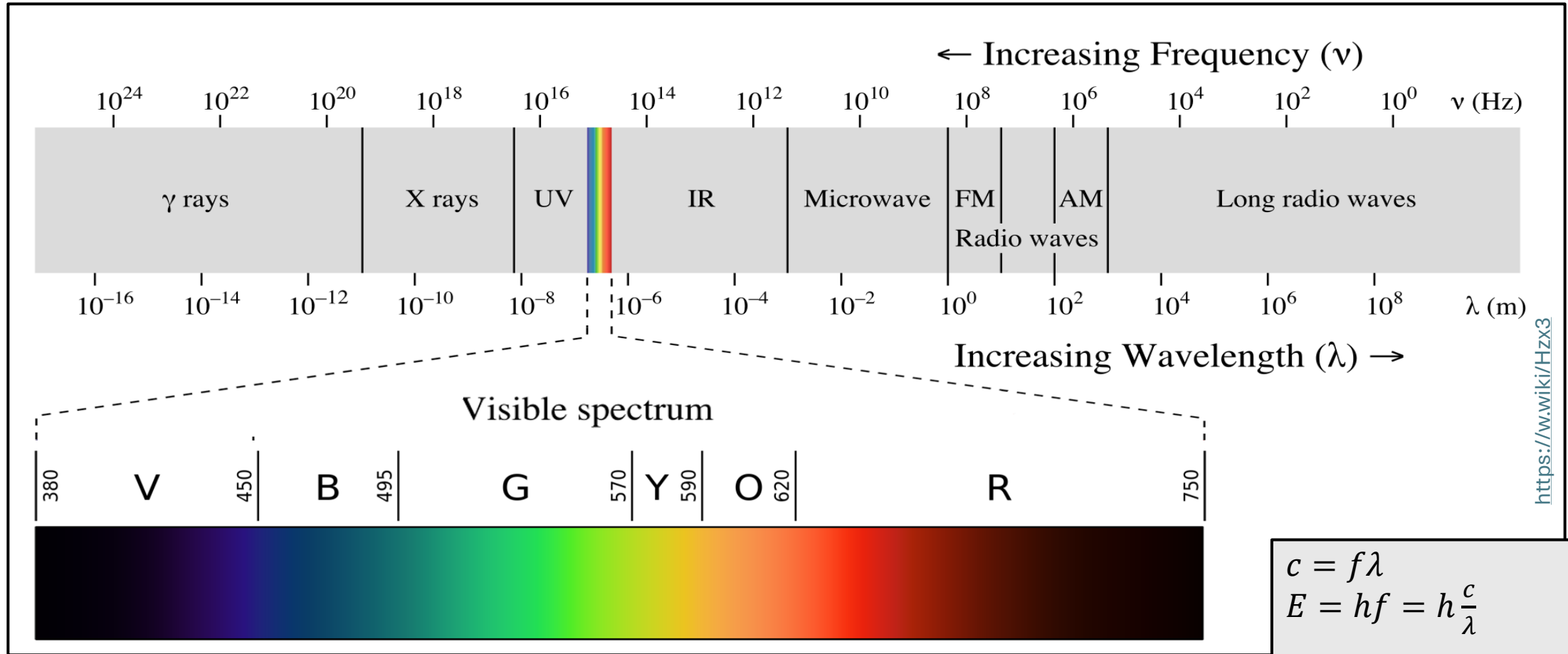
$$\nabla \cdot \vec{E} = \frac{\rho}{\epsilon_0} \quad \text{: Gauss's law (electric field)}$$

$$\nabla \cdot \vec{B} = 0 \quad \text{: Gauss's law (Magnetic field)}$$

$$\nabla \times \vec{E} = -\frac{\partial \vec{B}}{\partial t} \quad \text{: Faraday's law}$$

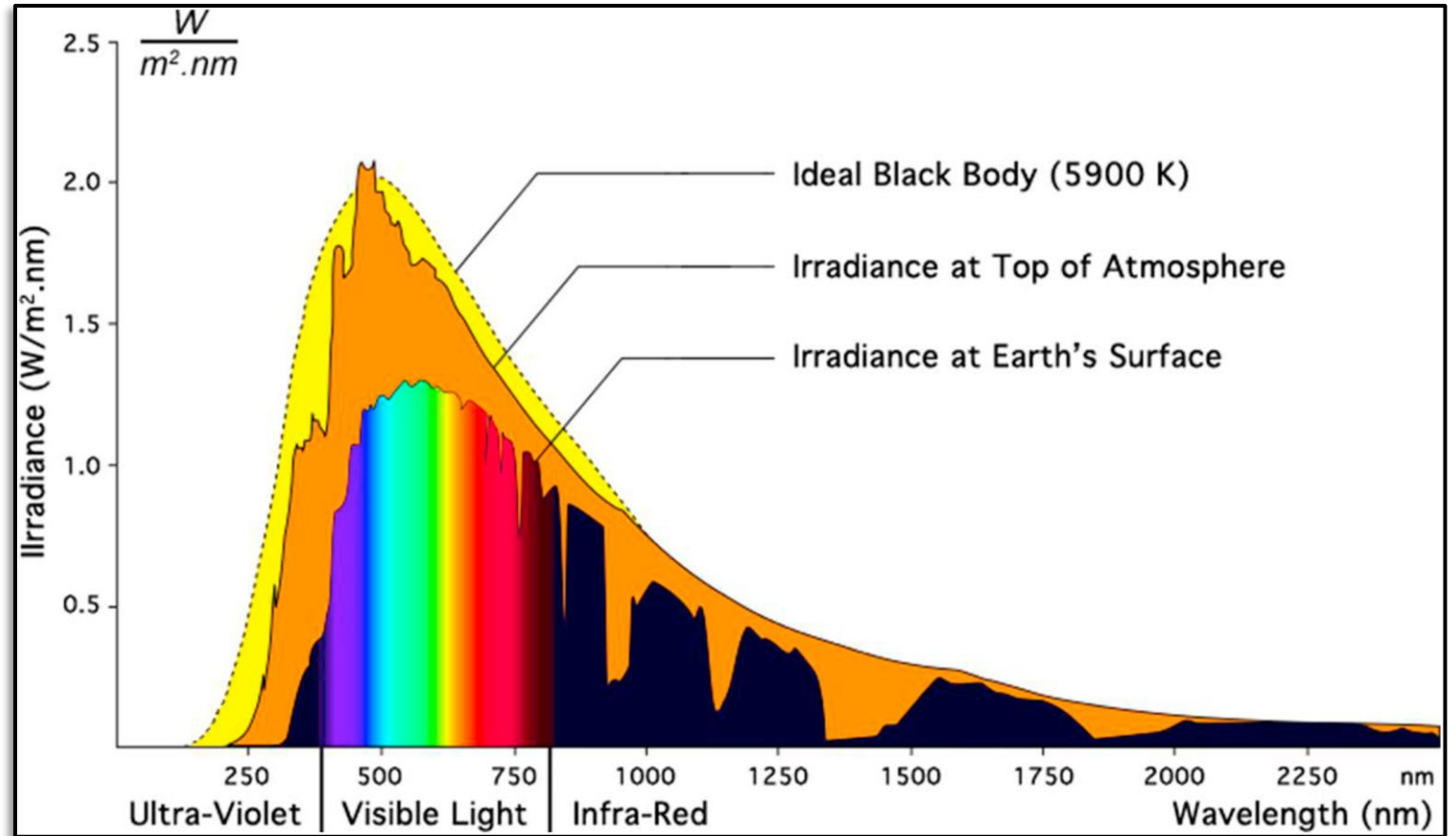
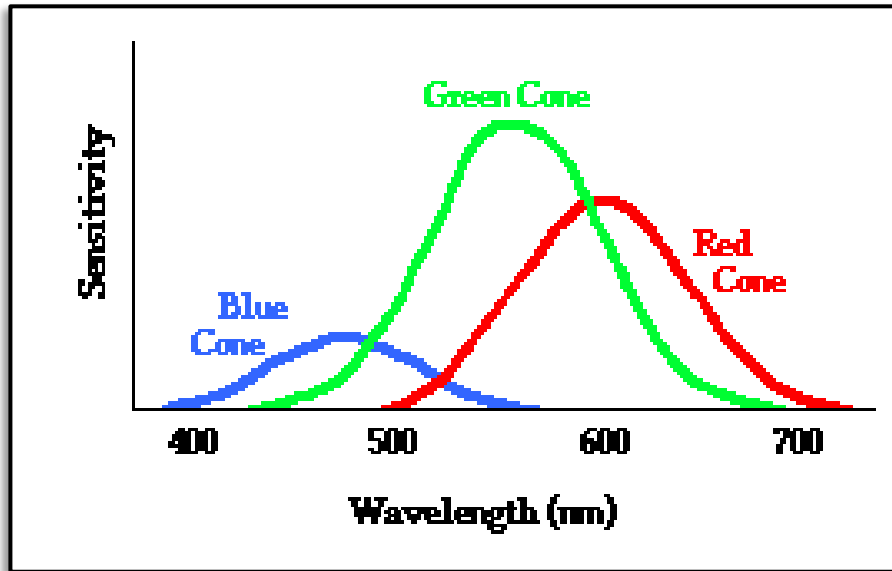
$$\nabla \times \vec{B} = \mu_0 \left(\vec{J} + \frac{\partial \vec{E}}{\partial t} \right) \quad \text{: Ampere's law}$$

Electromagnetic spectrum



Electromagnetic spectrum

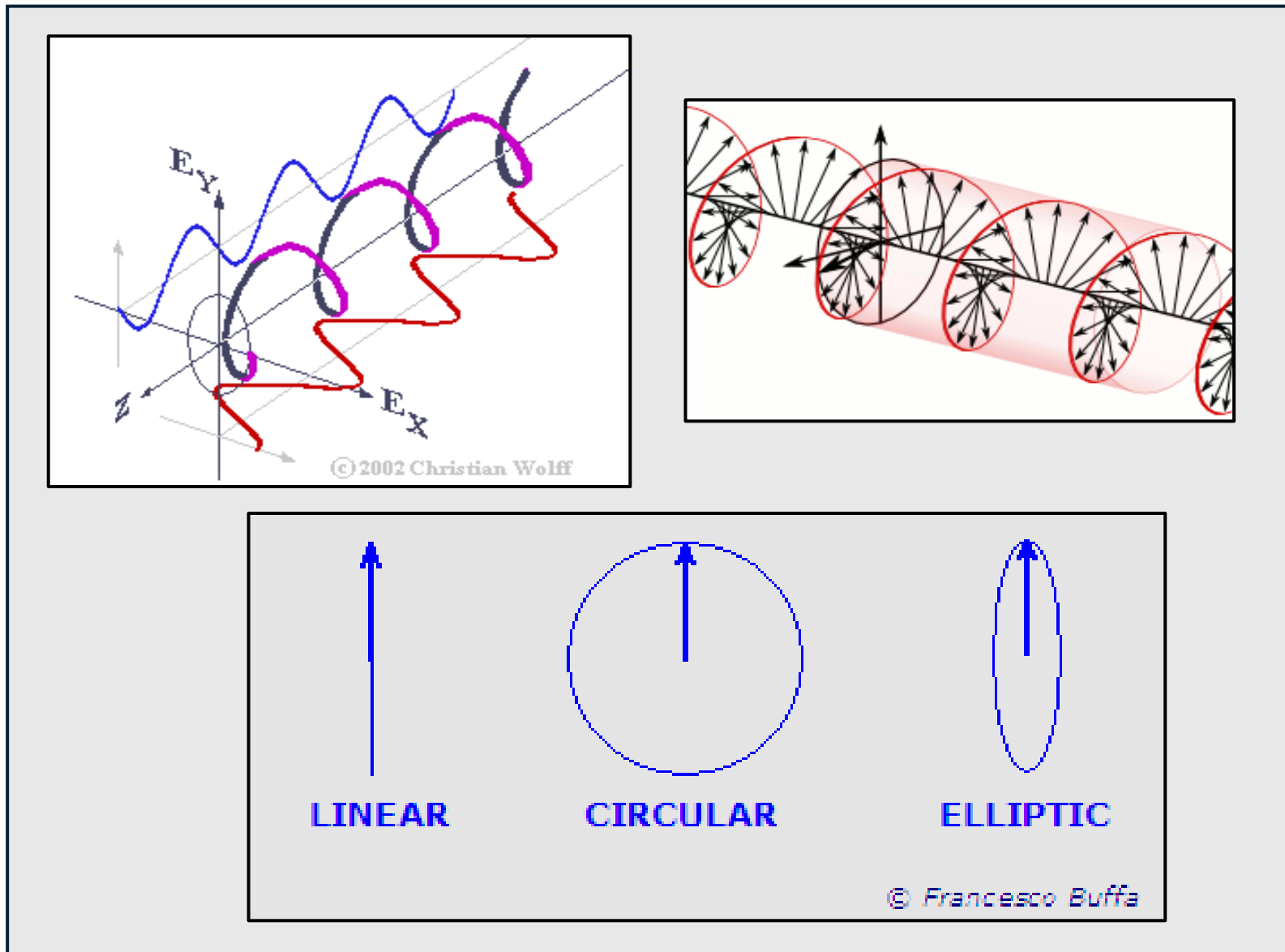
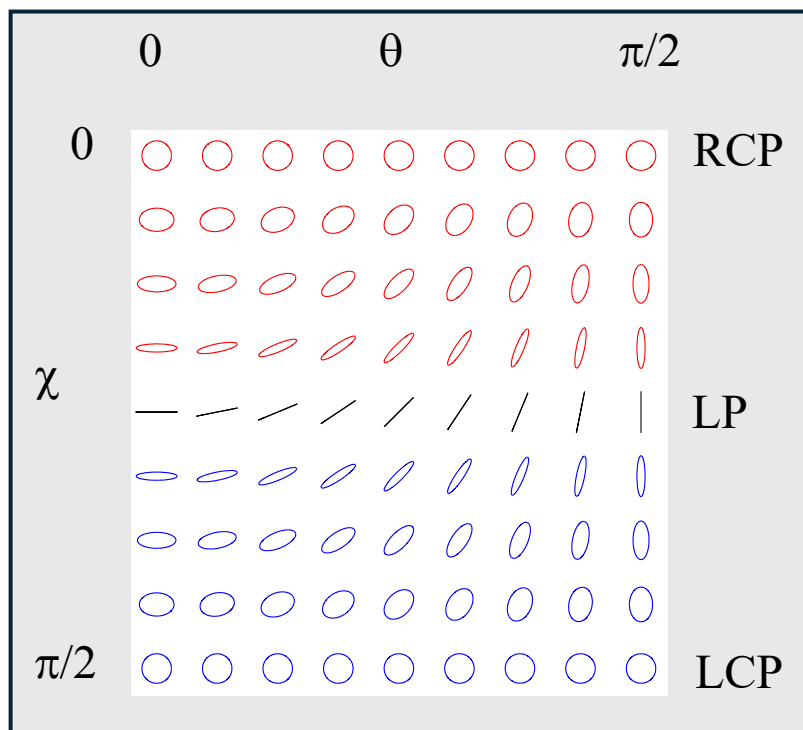
human eye cone sensitivity curve



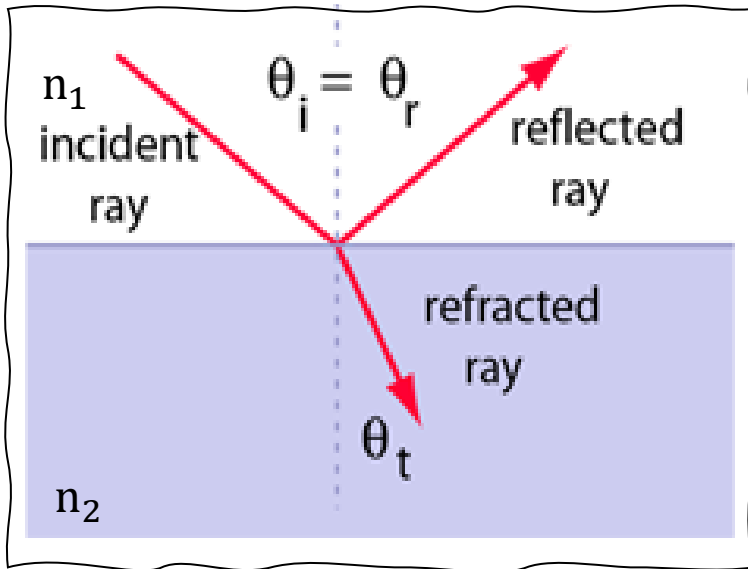
EM field - Polarization

EM wave is a **transverse** wave.
Electric field vector **oscillations**
determines the **polarization**:

Linear, Circular, Elliptical



EM field - propagation

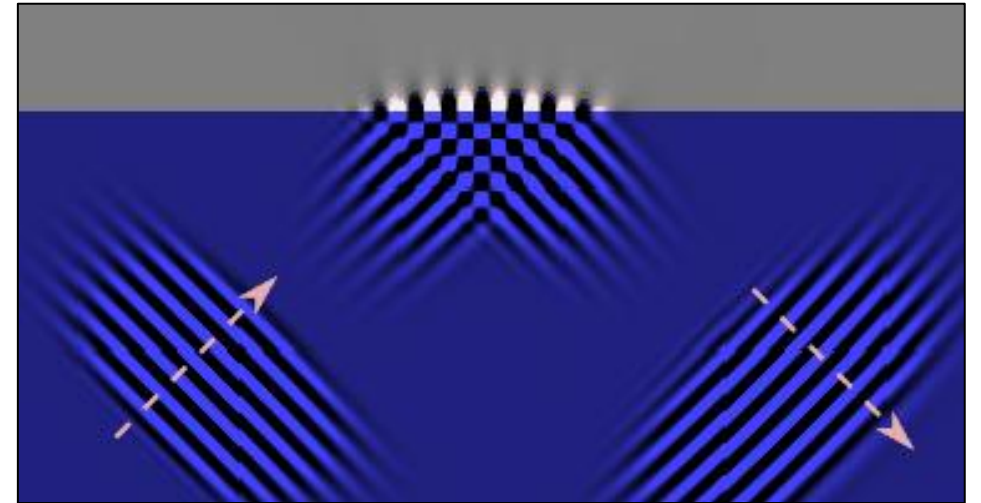


<http://hyperphysics.phy-astr.gsu.edu/hbase/phyopt/reflectcon.html#c1>

Reflection

$$\theta_i = \theta_r$$

Reflection



<https://commons.wikimedia.org/wiki/File:Internal-reflection.gif>

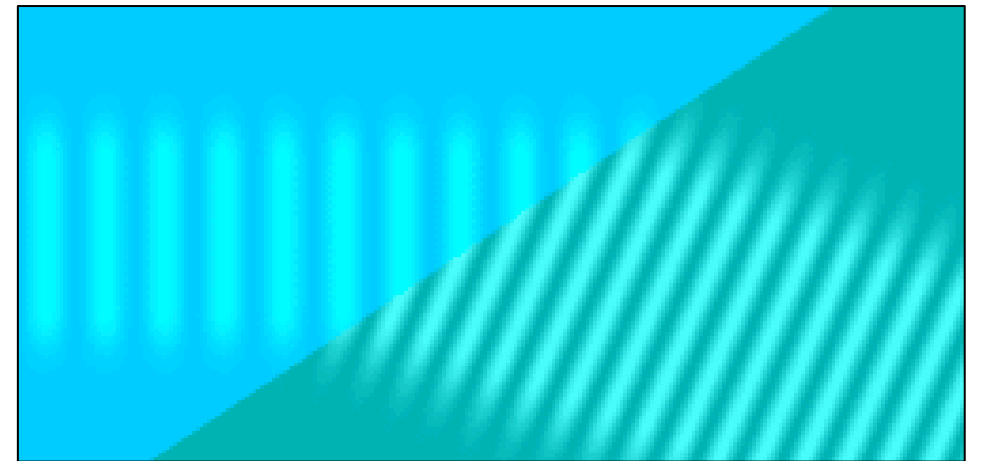
n: Refractive index
is the parameter with which light slows down while propagating in a medium.
The ratio speed of light in vacuum with respect to medium.

In vacuum: $c = \lambda f_{vacuum}$

In medium: $V = c/n$, $n > 1$

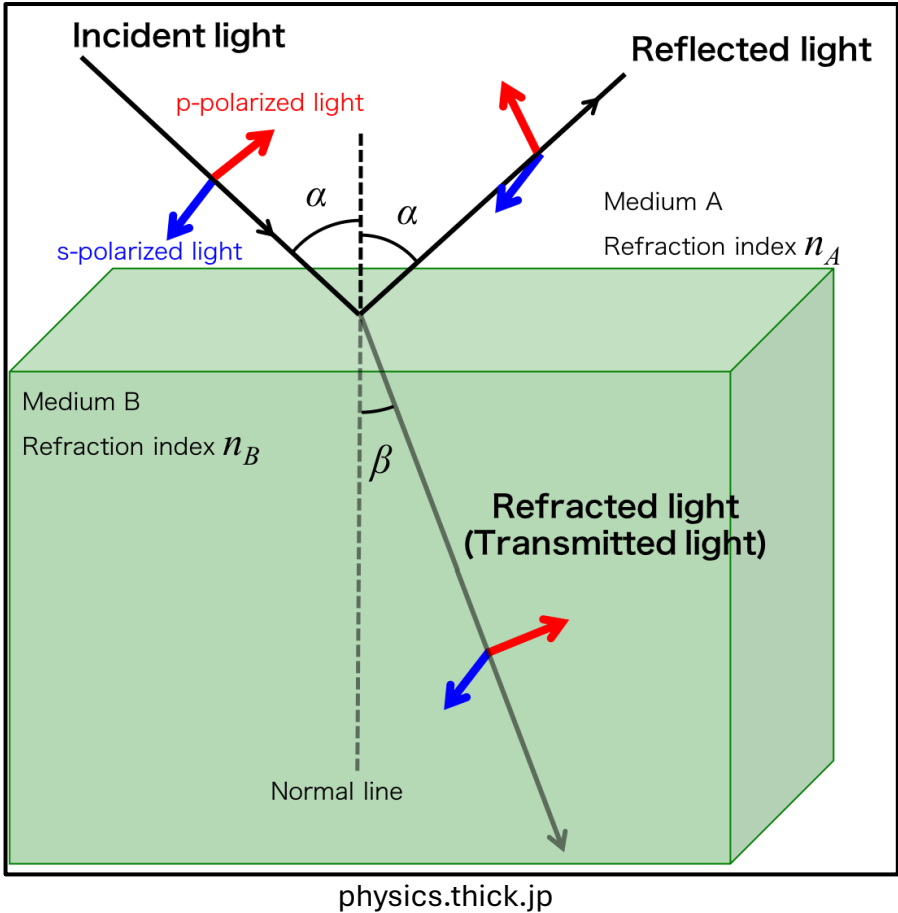
Refraction: Snell's law
 $n_1 \sin \theta_i = n_2 \sin \theta_t$

Refraction

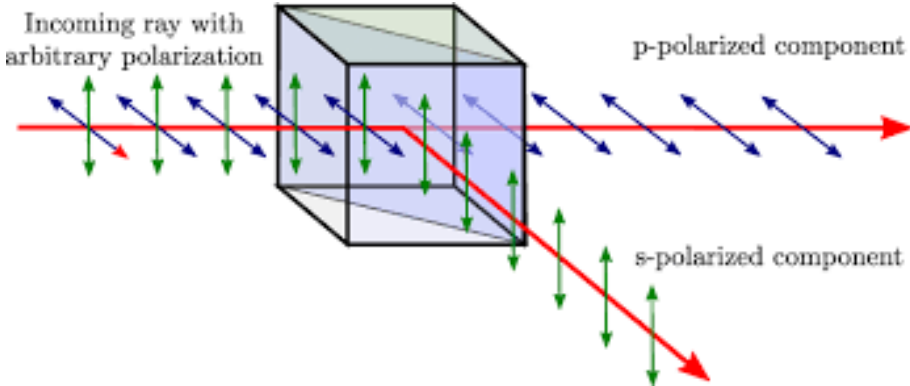


<https://en.wikipedia.org/wiki/Refraction>

Polarization effect in Reflection and Refraction

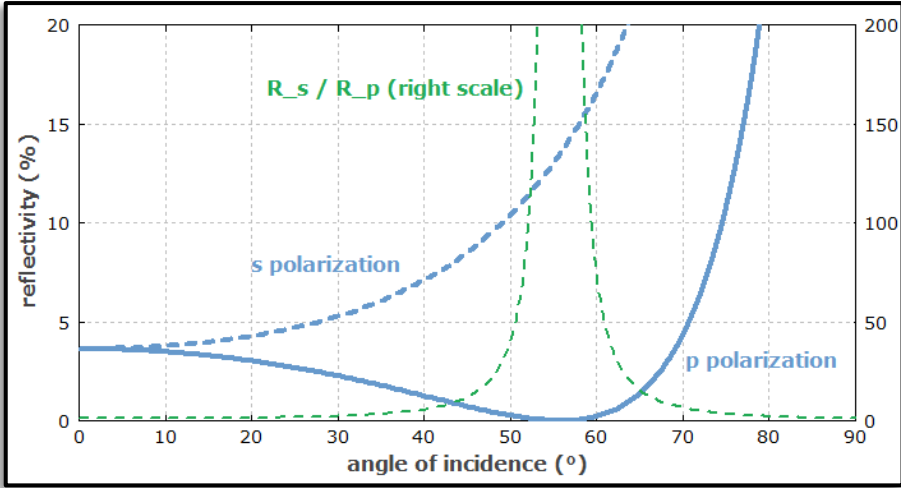


Polarizing BS in microscopes



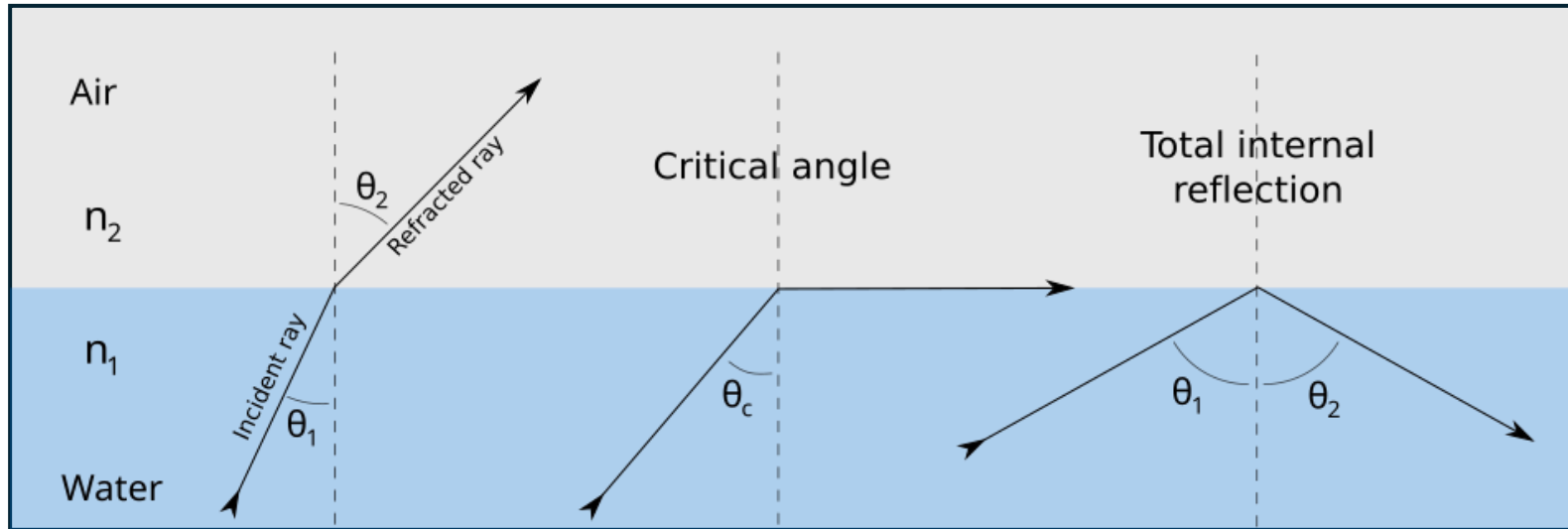
Refraction simulation

Fresnel equations



EM field - propagation

Refractive Index and Total Internal Reflection



Material	n
air	1
water	1.33
PBS	1.37
Immersion oil	1.52
glass	1.46 - 1.8

[https://en.wikipedia.org/wiki/Reflection_\(physics\)#Laws_of_reflection](https://en.wikipedia.org/wiki/Reflection_(physics)#Laws_of_reflection)

Refractive index of most biological specimen is around **1.4**

In vacuum: $c = \lambda f_{vacuum}$

In medium: $V = c/n$

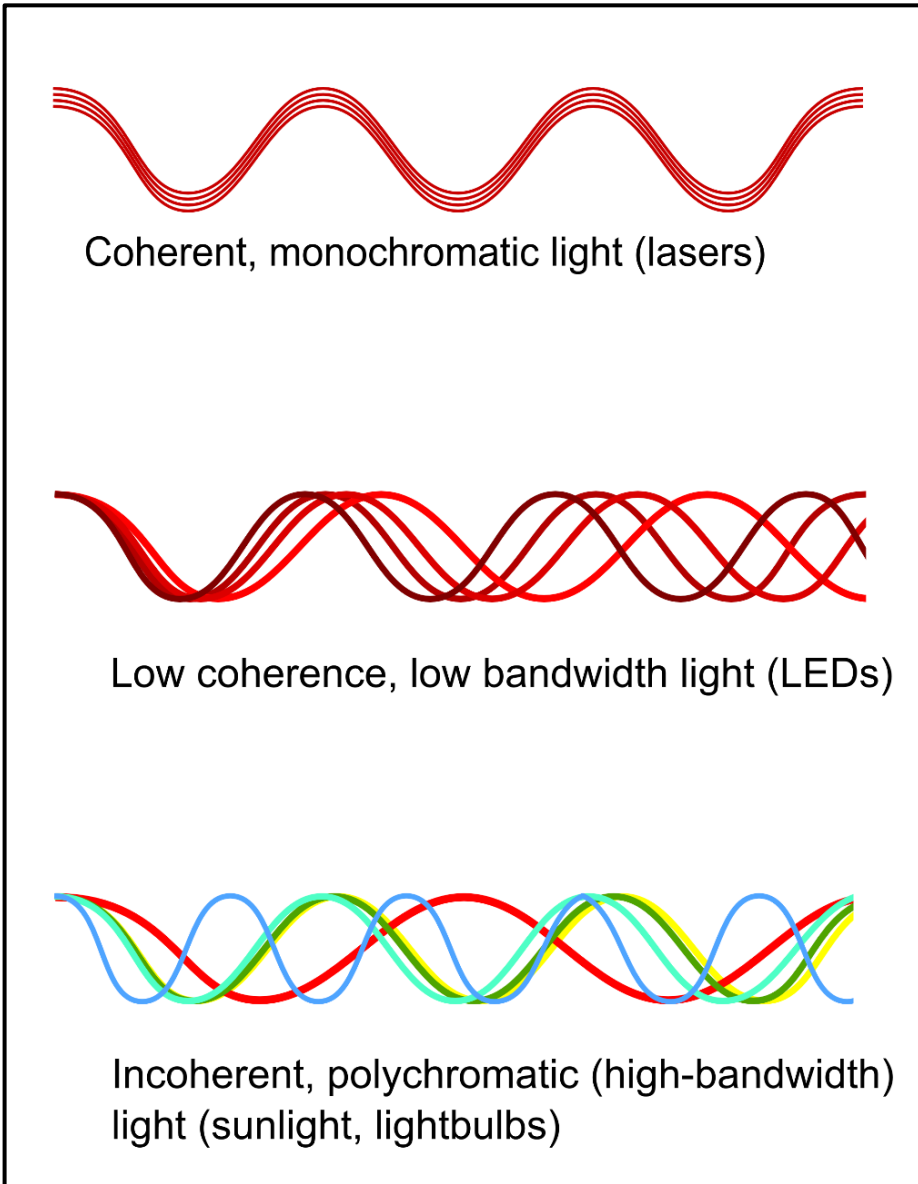
$f_{vacuum} = f_{medium}$ (function of source)

$E_{photon} = hf$ (Energy of light photon)

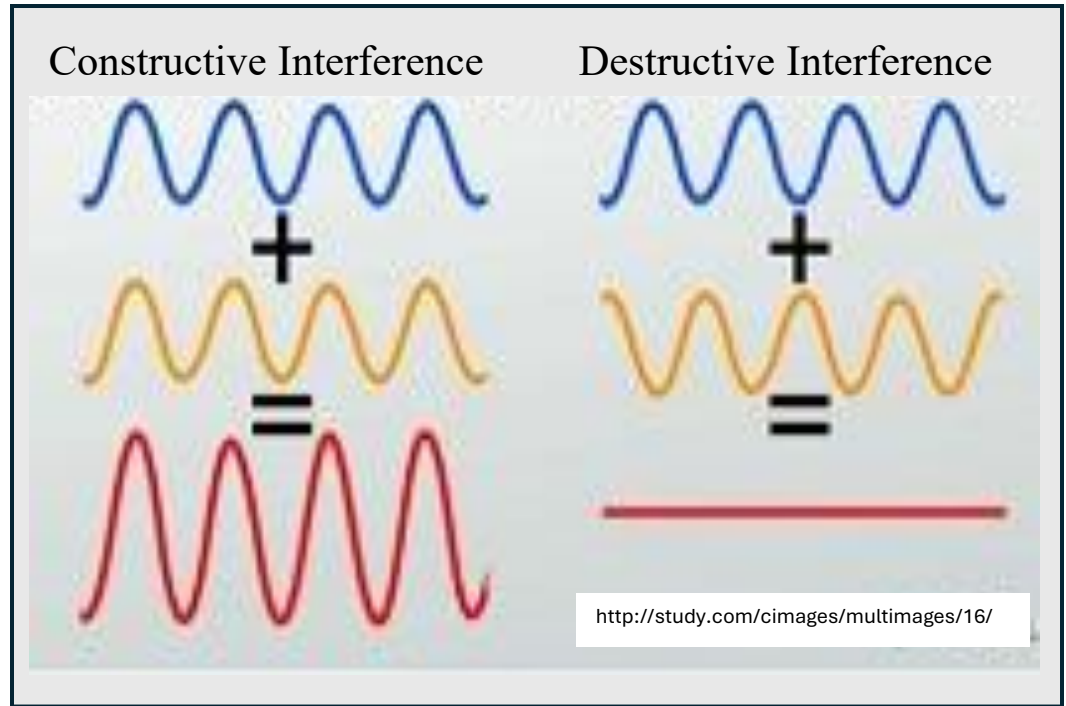
The color that our eyes perceive: Energy \rightarrow frequency

Refractive index, $n = \frac{c}{v}$ is a function of the **wavelength**

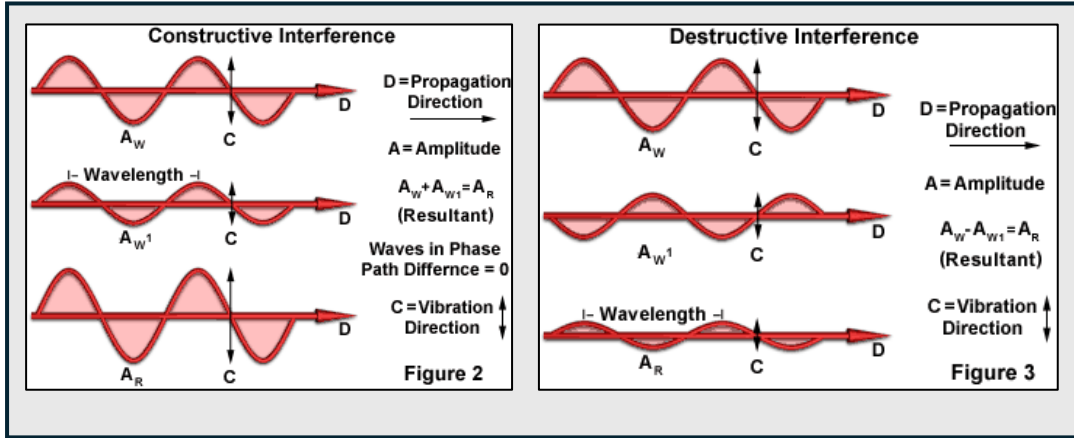
EM field - Coherence and Interference



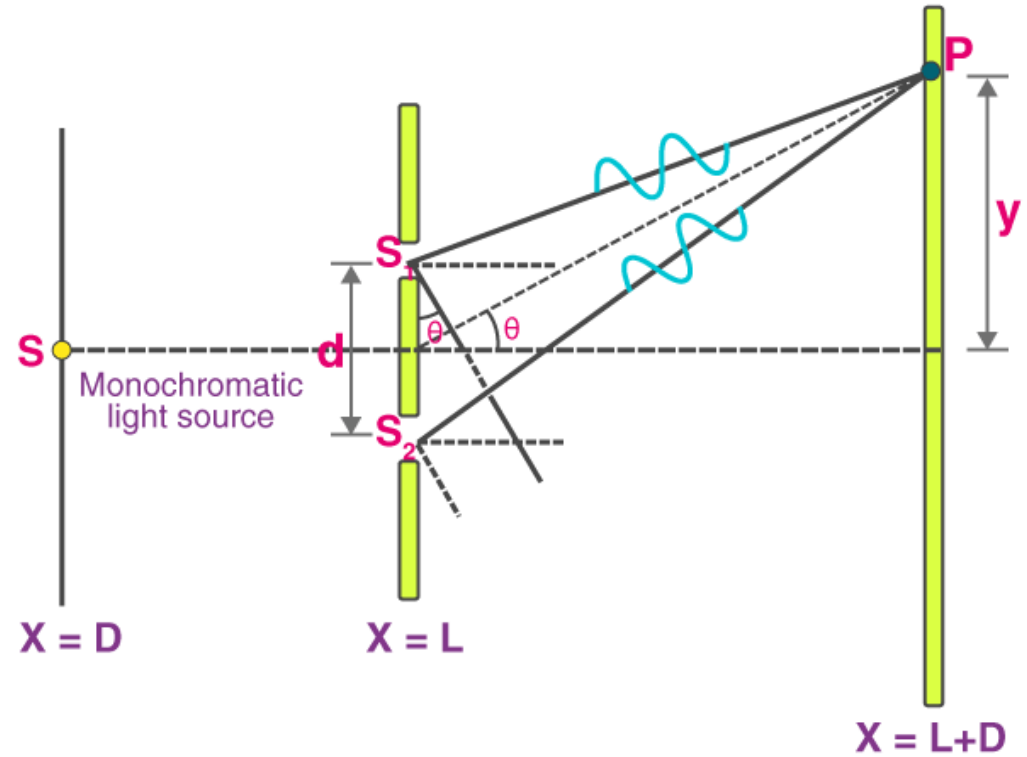
- Coherent light: well-defined relationship in phase at different points in space (wavelength dependent)
- Generates constructive and destructive interference- useful for looking at path-length differences and moving light-scatterers



Interference and Young's double slit experiment

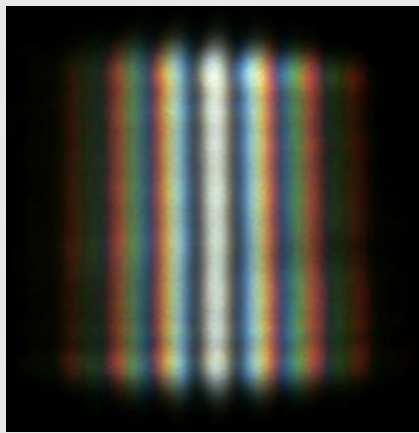


<https://evidentscientific.com/en/microscope-resource/knowledge-hub/lightandcolor/interference>



© Byjus.com

double slit
interference of
sunlight



For small θ : $\tan \theta \approx \theta \approx \sin \theta \approx \frac{\lambda}{d}$

EM field - Diffraction

Superposition of many interferences from an aperture (**wavelength dependent**)

MATLAB app

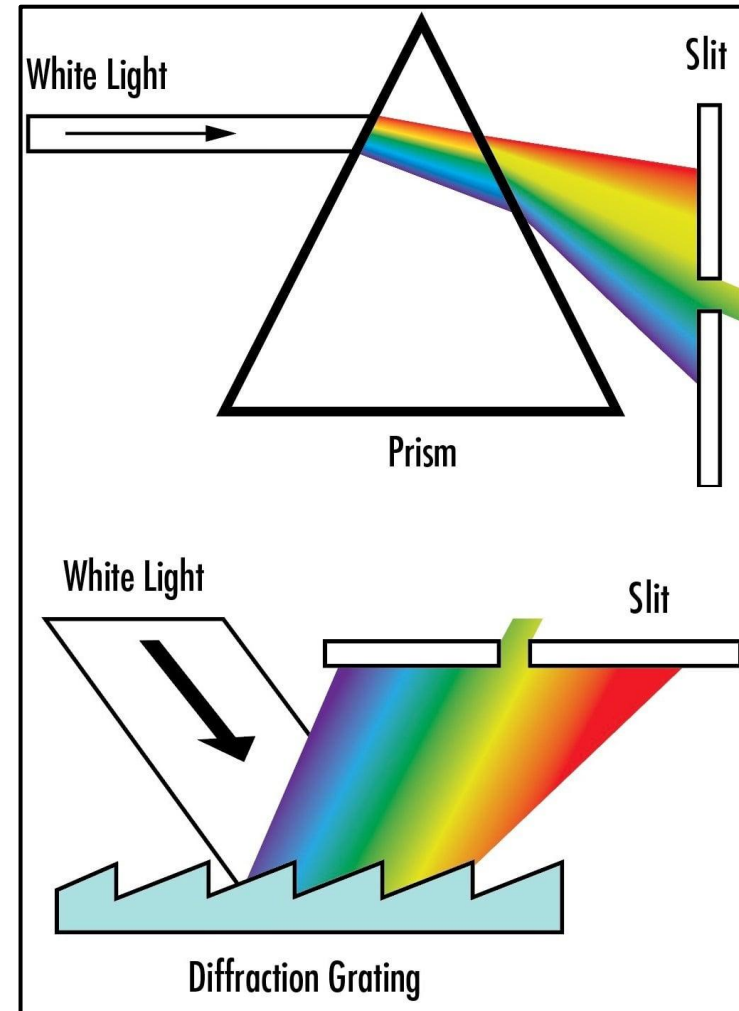
[Most accurate approximation]

Rayleigh-Sommerfeld

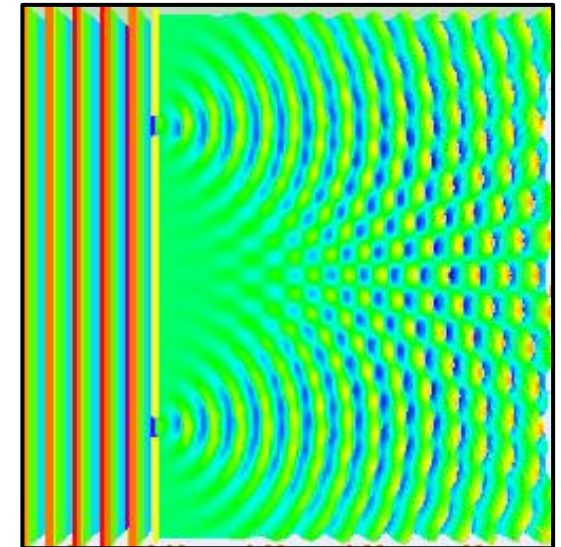
Fresnel

Fraunhofer

[Least accurate approximation].



Double slit simulation

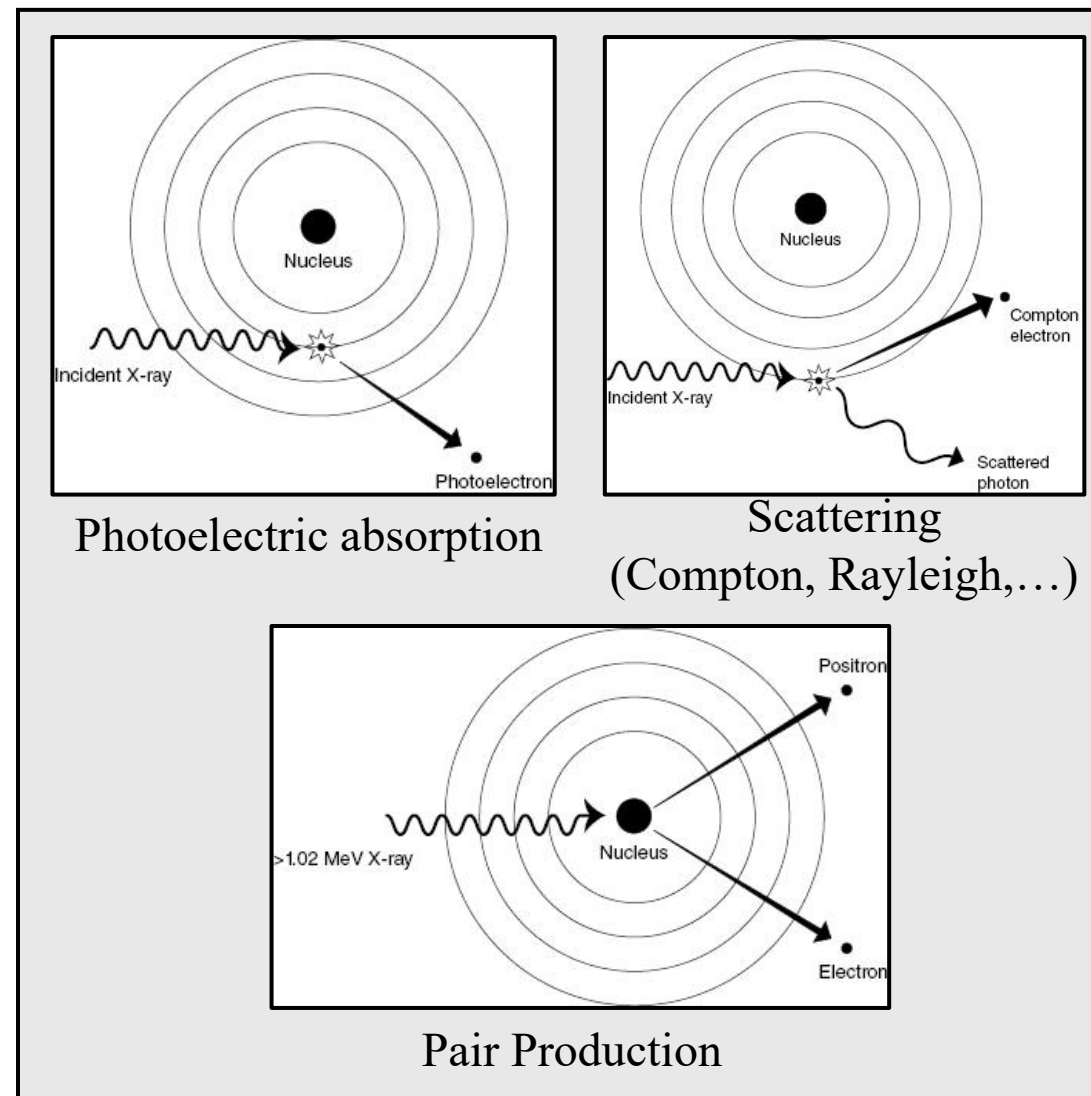
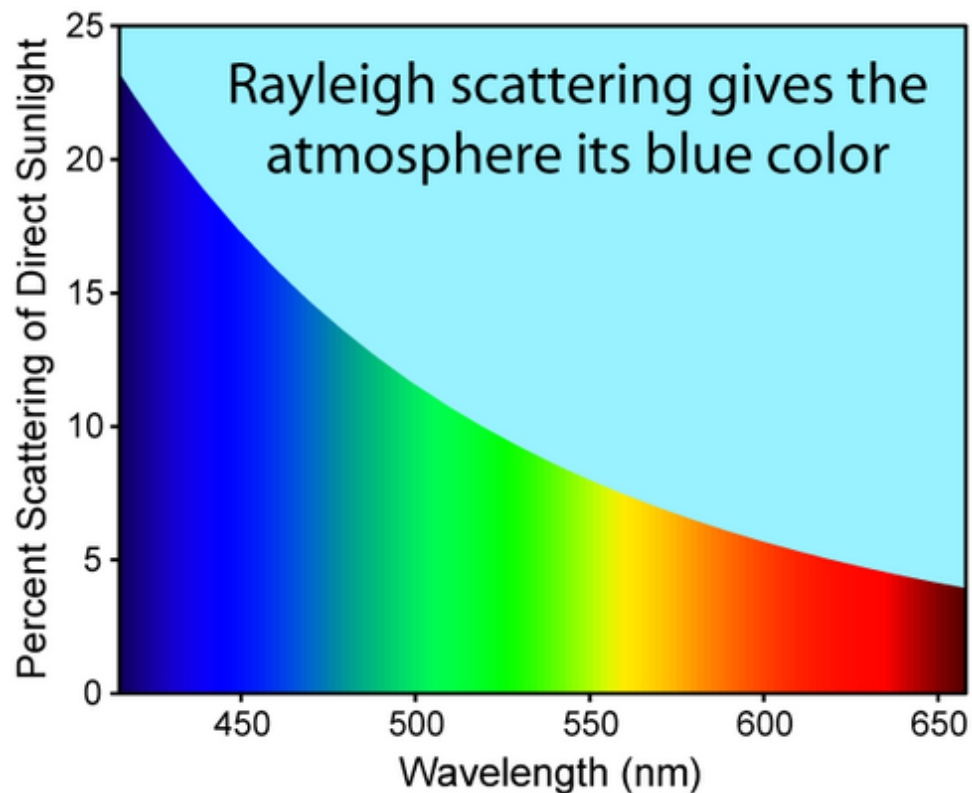


dispersion prisms separate wavelengths through refraction (top)
diffraction gratings separates wavelengths through diffraction (bottom)

EdmundOptics

Light Interaction with Matter

Longer Wavelength : Rayleigh scattering ↓

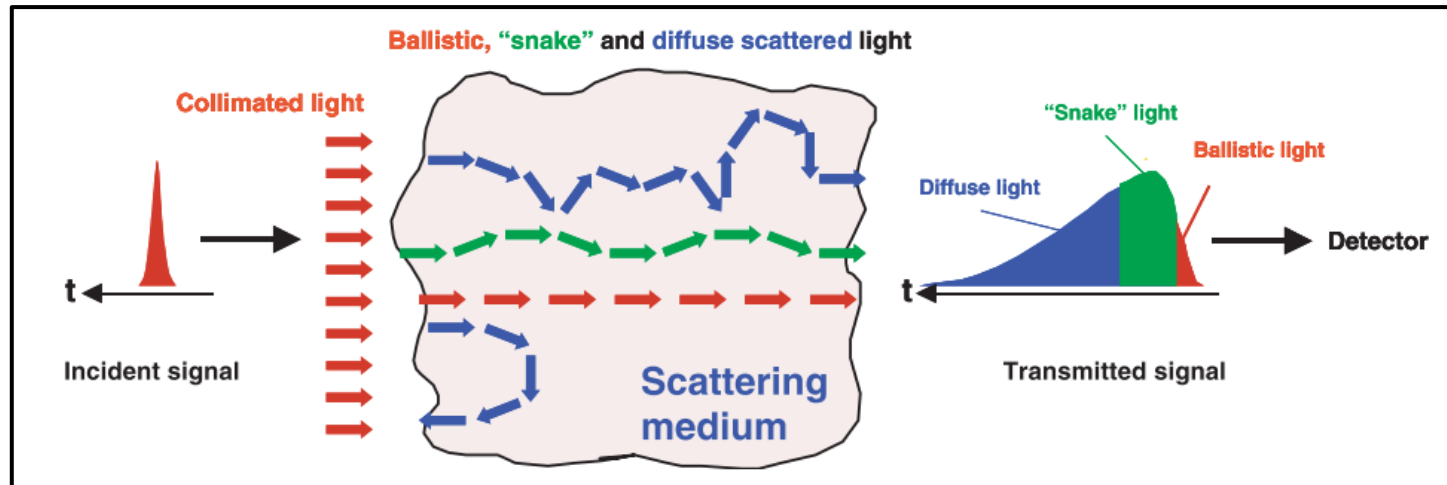
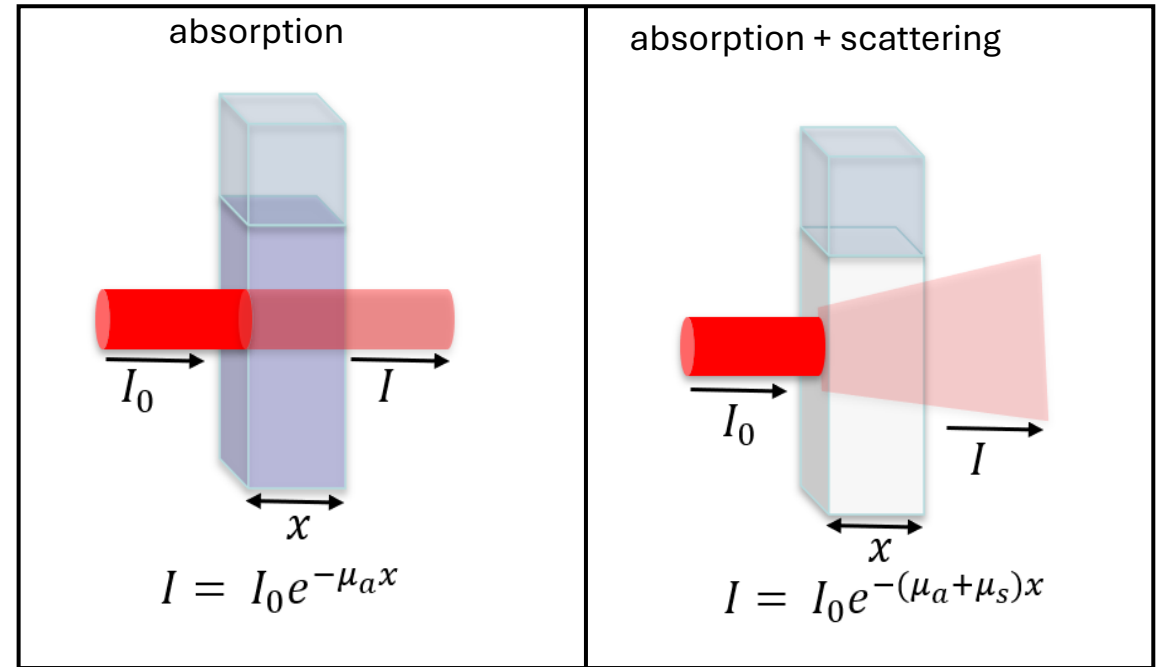


<https://radiologykey.com/4-radiation-interactions-with-tissue/>

Light Interaction with Matter

Light Propagation in Tissue

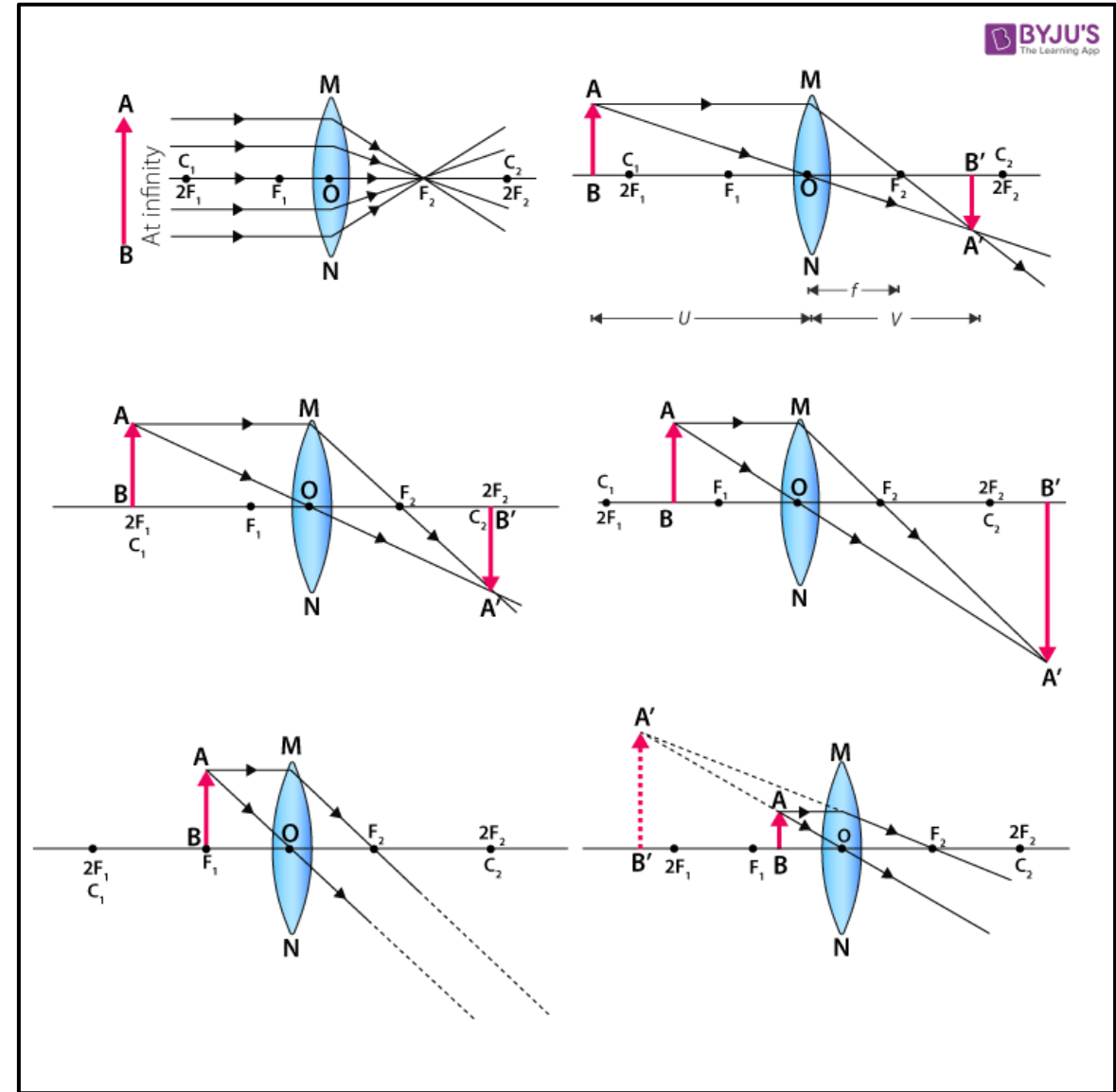
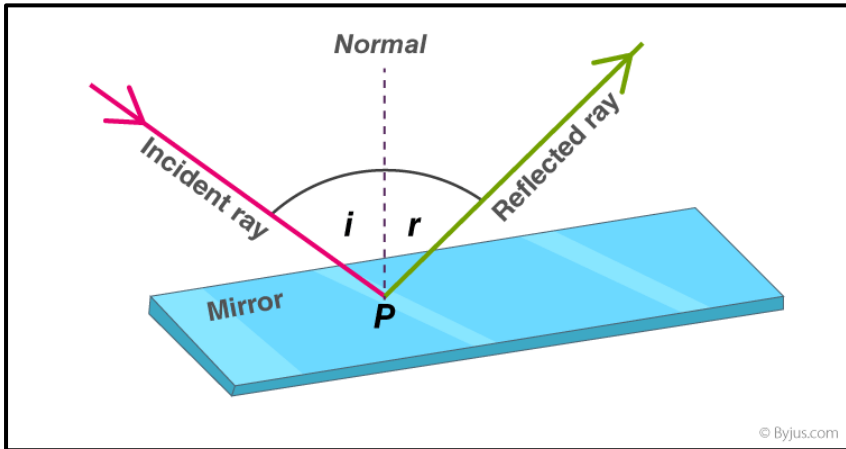
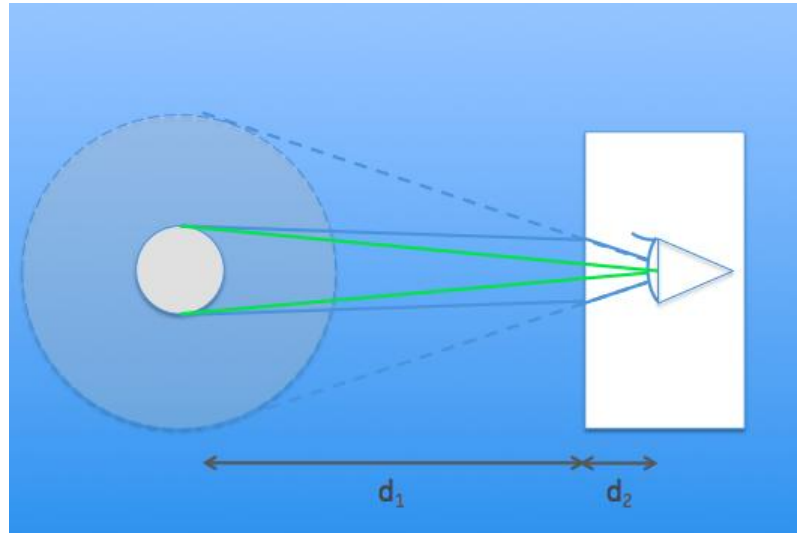
EM wave (in material)
<https://emanim.szialab.org/index.html>



C Dunsby and P M W French 2003 J. Phys. D: Appl. Phys. 36 R207

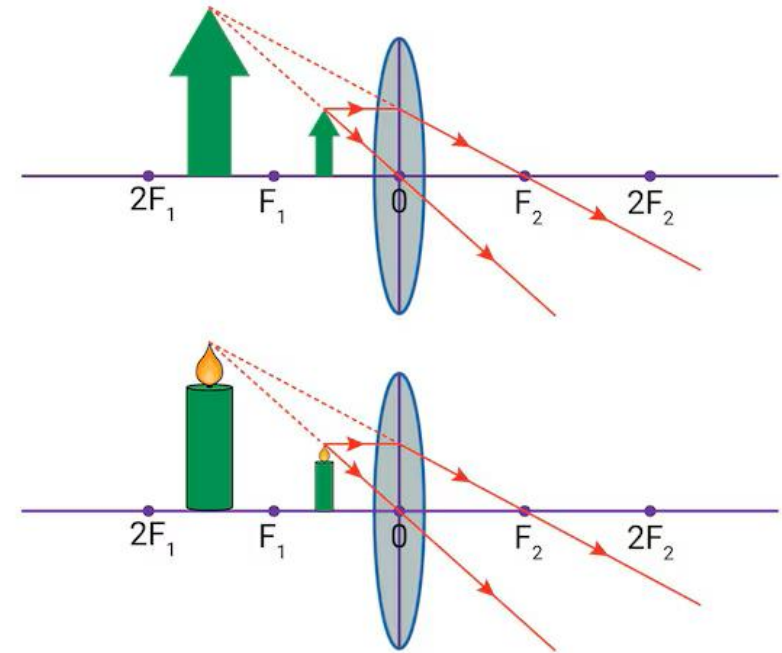
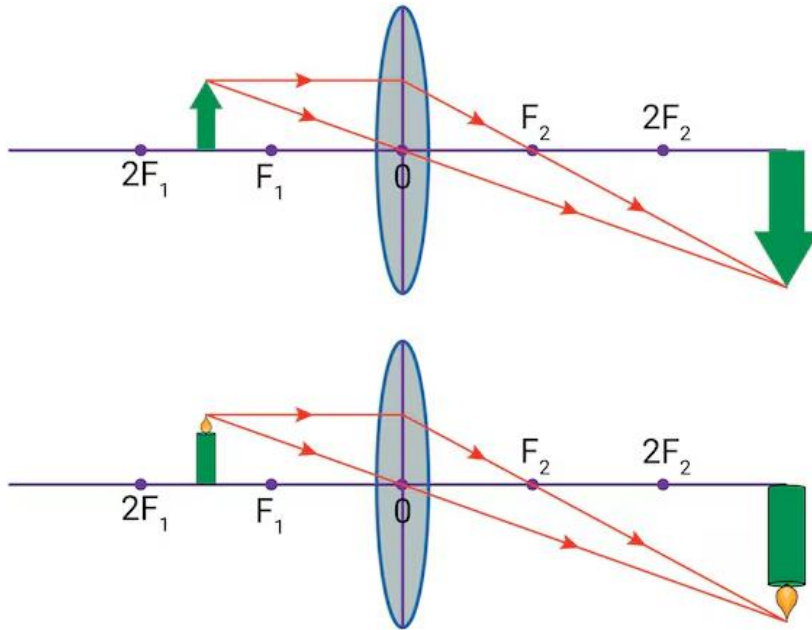
light ray manipulation

Refraction, Reflection, Image formation, (De)Magnification



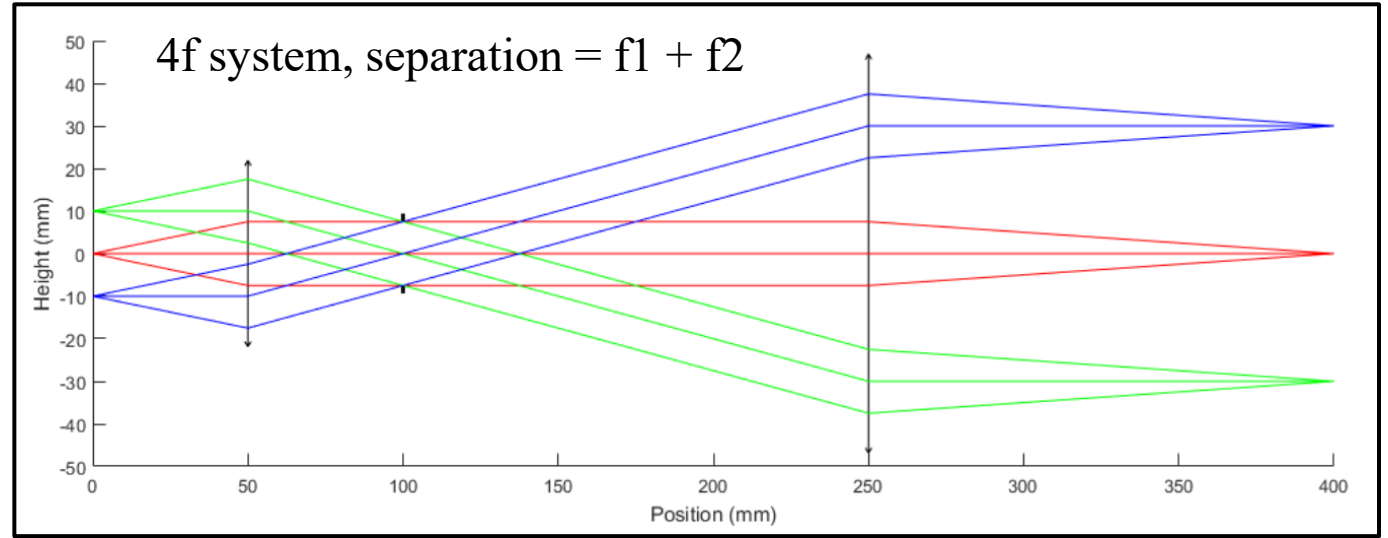
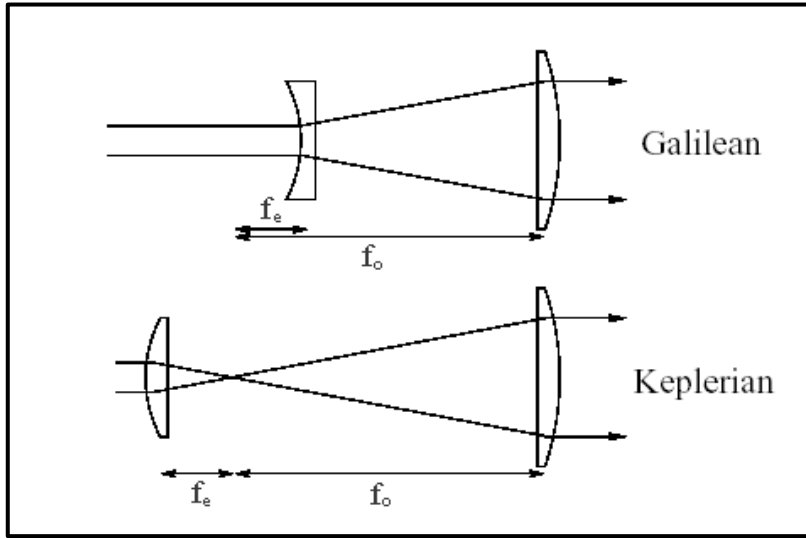
light ray manipulation

Ray diagram for a converging lens

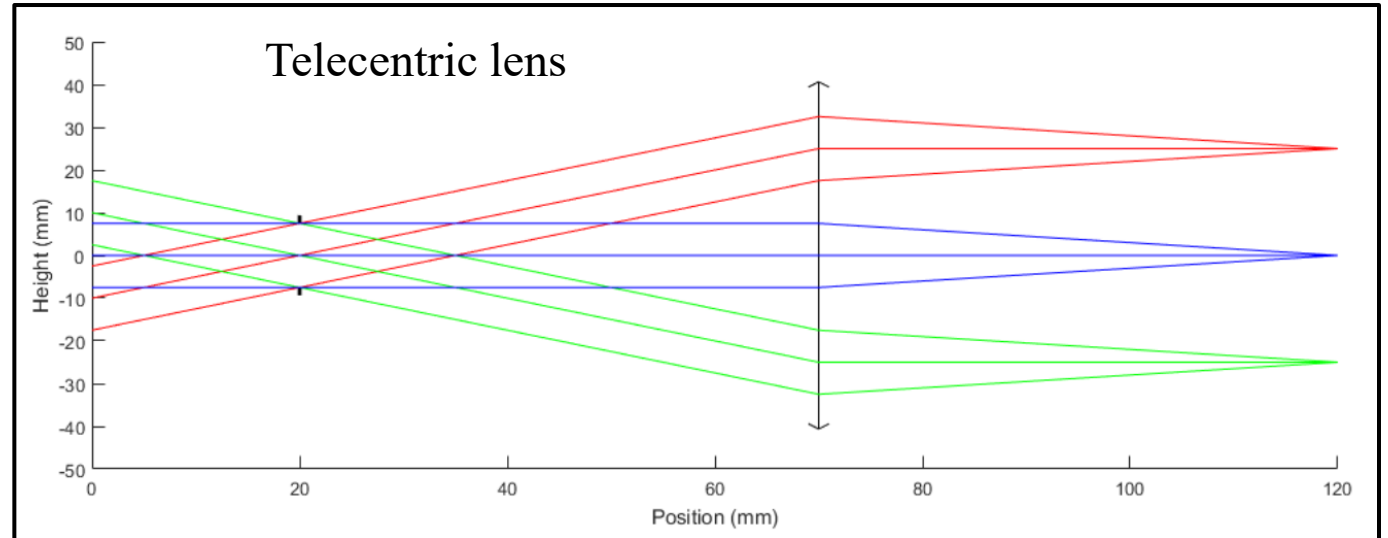
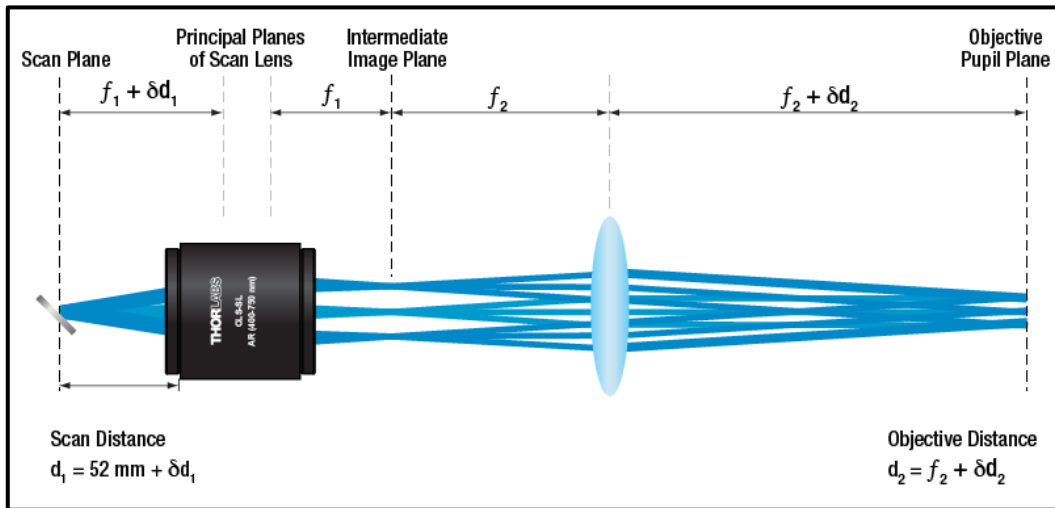


1. Rays parallel to symmetry axis (optical axis) get focused (**focal point**).
2. Rays crossing the center point of the lens are not refracted.
3. Rays crossing the focal point, refract parallel to the optical axis.

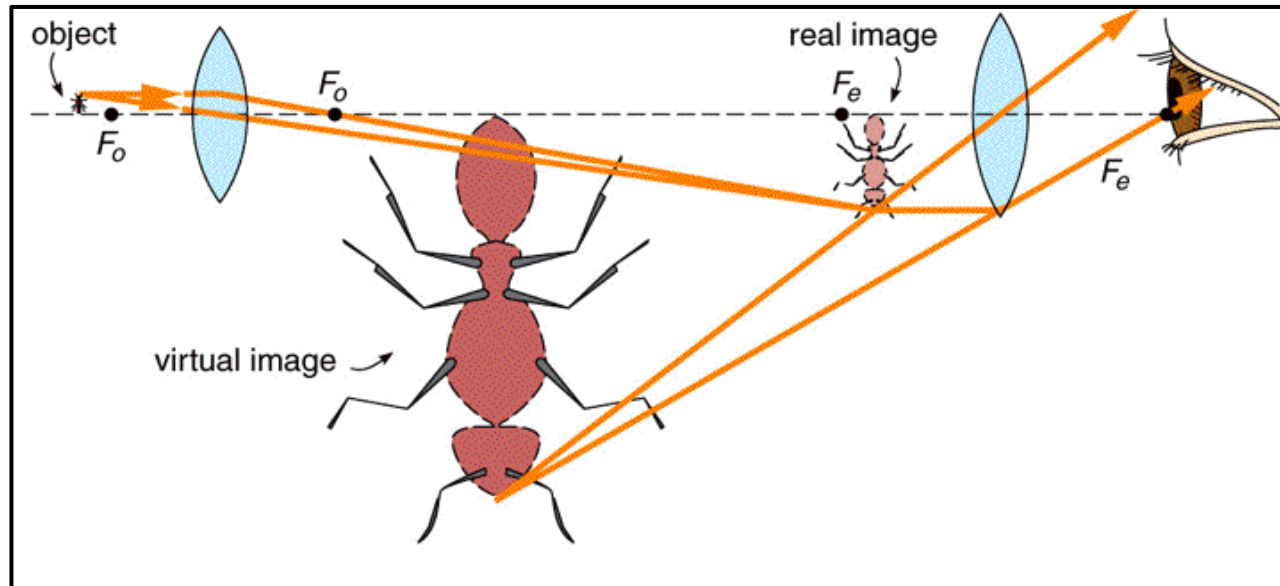
light ray manipulation – 4f system, telescopes, telecentric scan, etc.



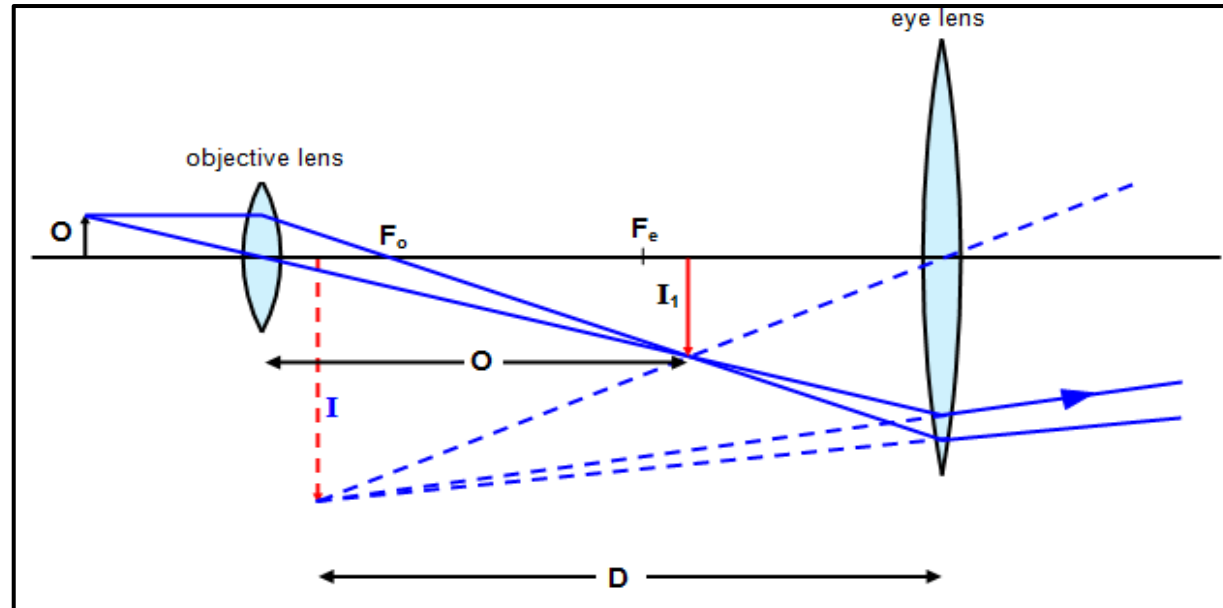
www.thepulsar.be



light ray manipulation – building microscope

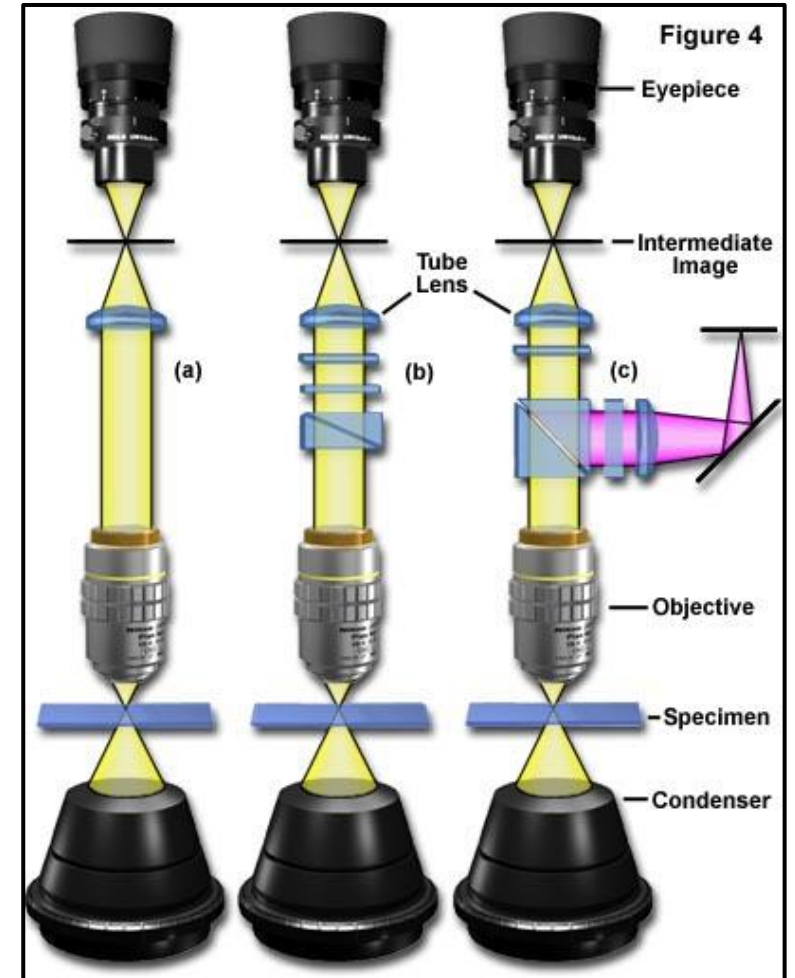
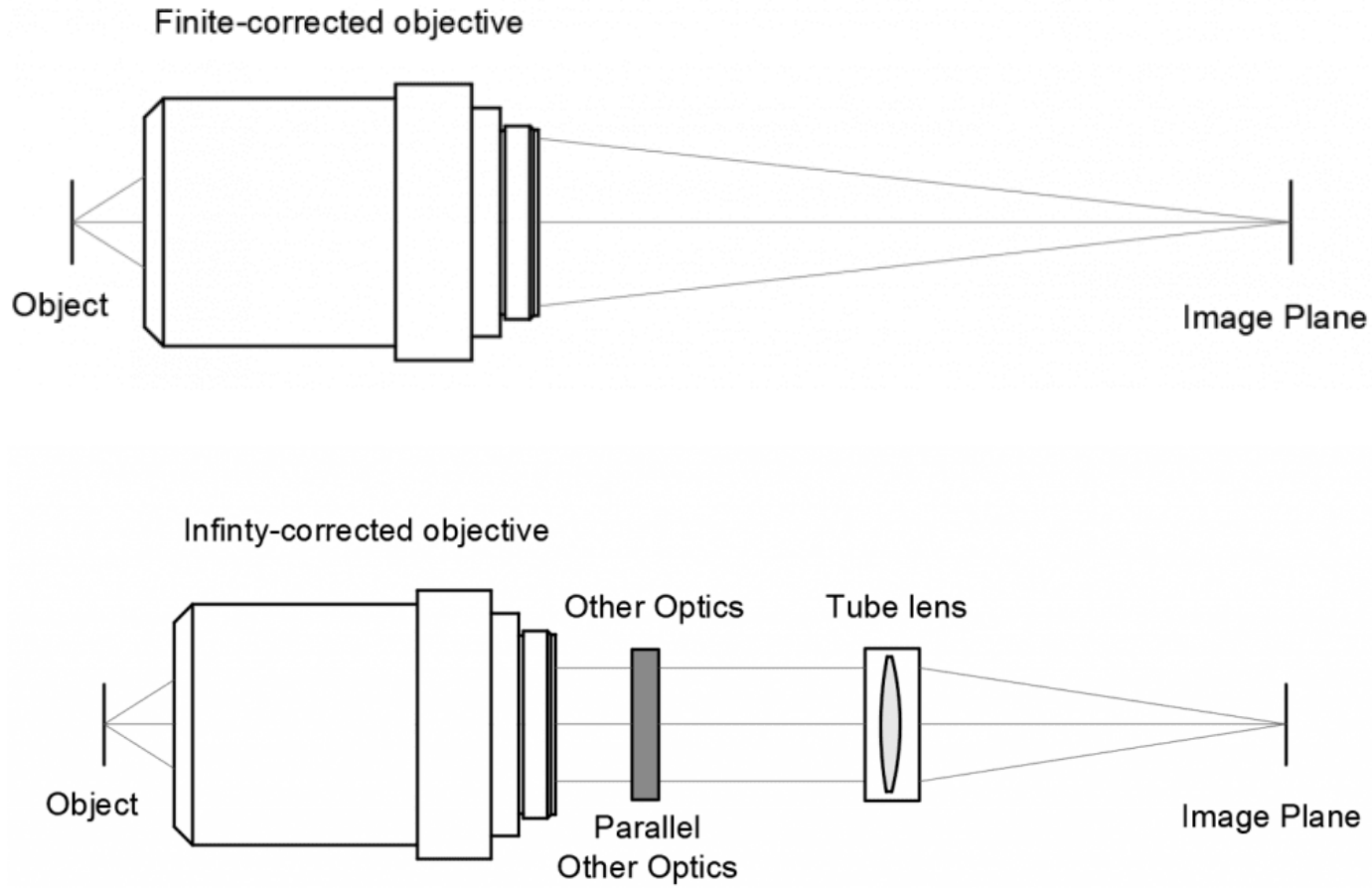


<https://www.schoolphysics.co.uk/>



<https://physics.stackexchange.com/>

light ray manipulation – building microscope

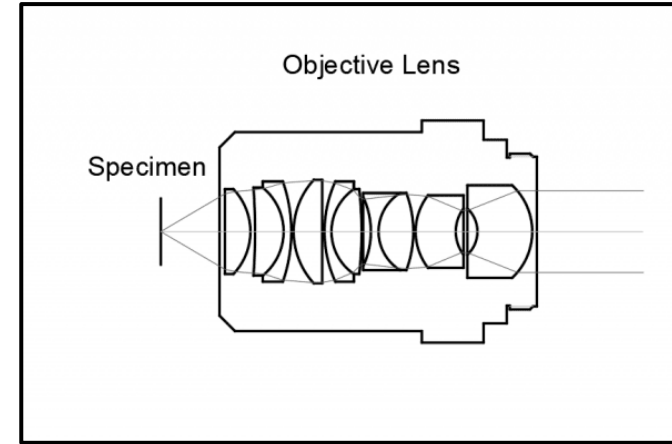


<https://micro.magnet.fsu.edu/>

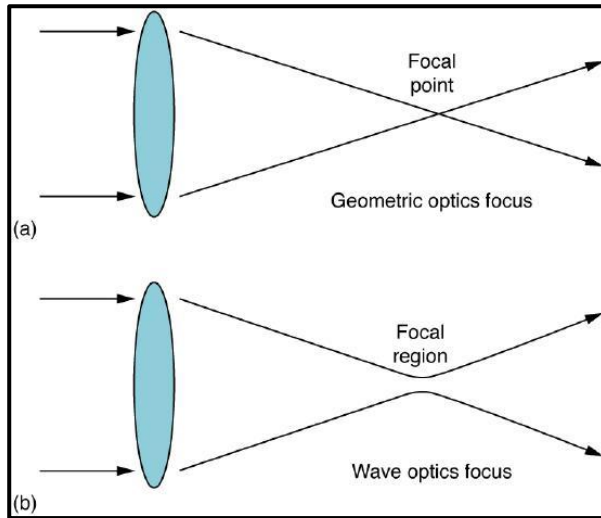
light ray manipulation – Objectives

Objectives come in various designs.

Dry, water, oil, NA, working distance, aberrations, etc.



Resolution and NA dependence

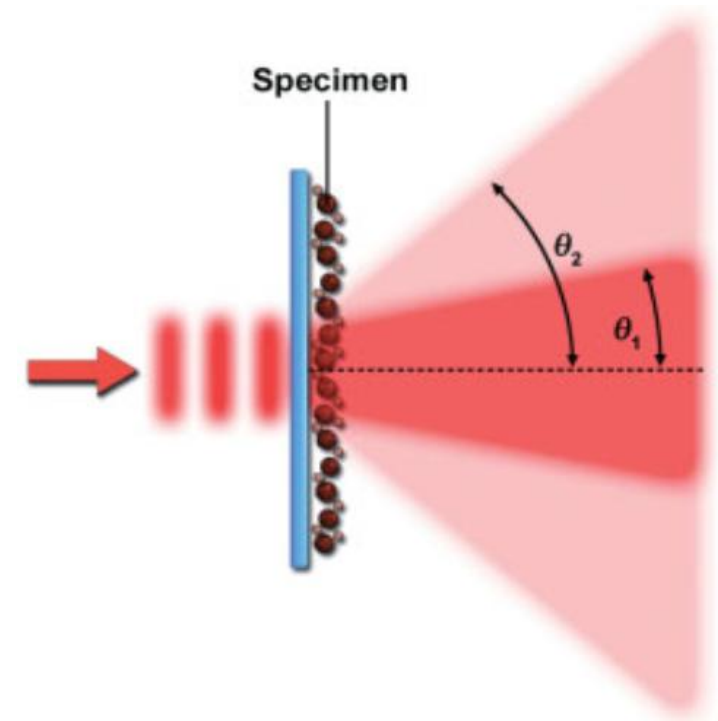


<https://phys.libretexts.org/>

$$\tan \theta \uparrow \approx \sin \theta \uparrow \approx \theta \uparrow \approx \frac{\lambda}{d \downarrow}$$

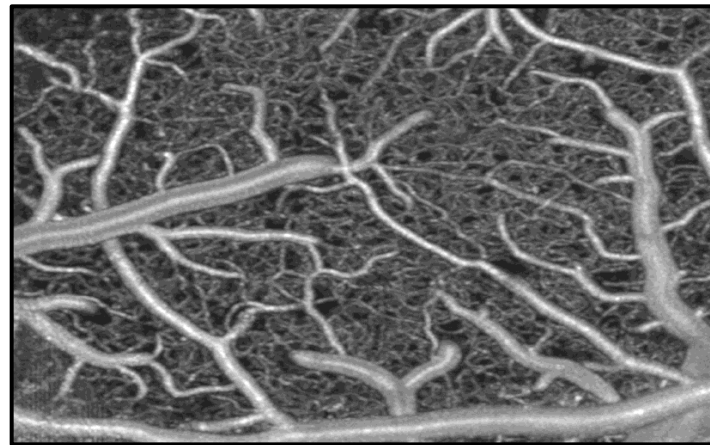
The angle of spreading (θ) is inversely proportional to the size of the particles

finer periodic structures leaves the sample at a **higher angle**.



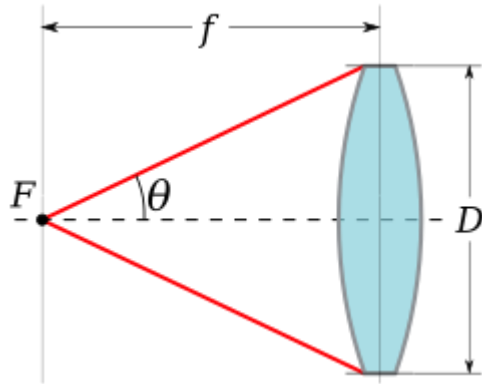
Douglas B. Murphy Michael W. Davidson,
Fundamentals of Light Microscopy..

Diffraction gratings Demo



Resolution and NA dependence

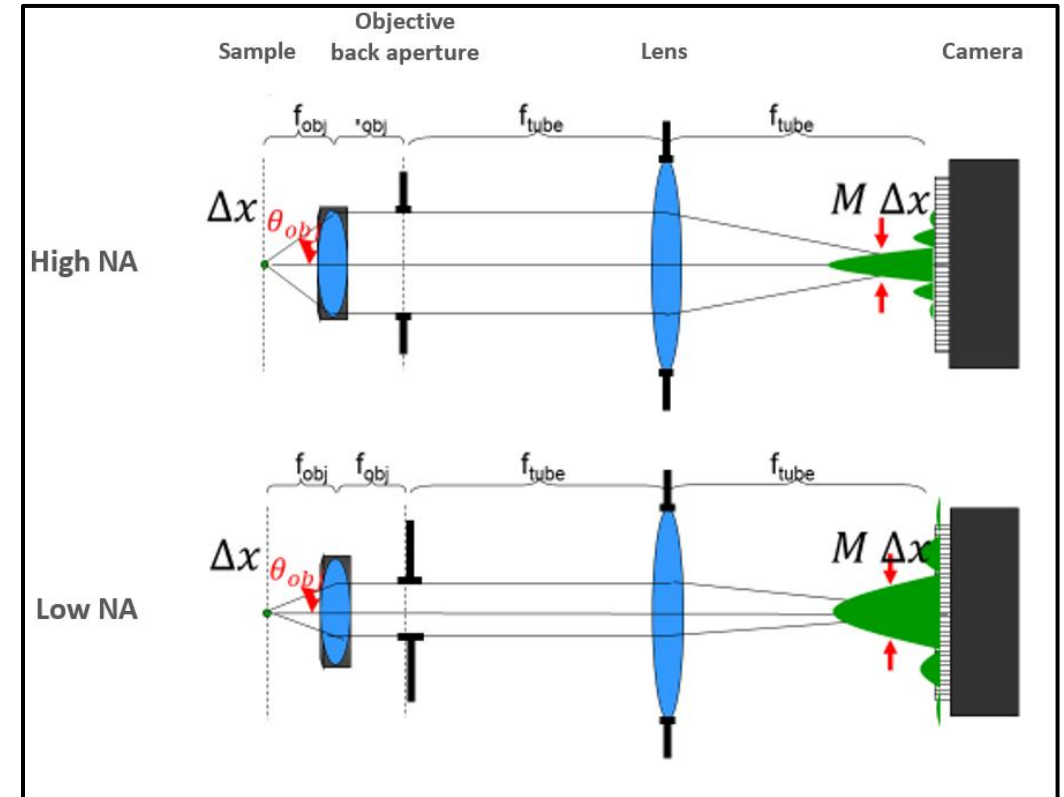
Numerical Aperture: $NA = n \sin \theta$



n : refractive index

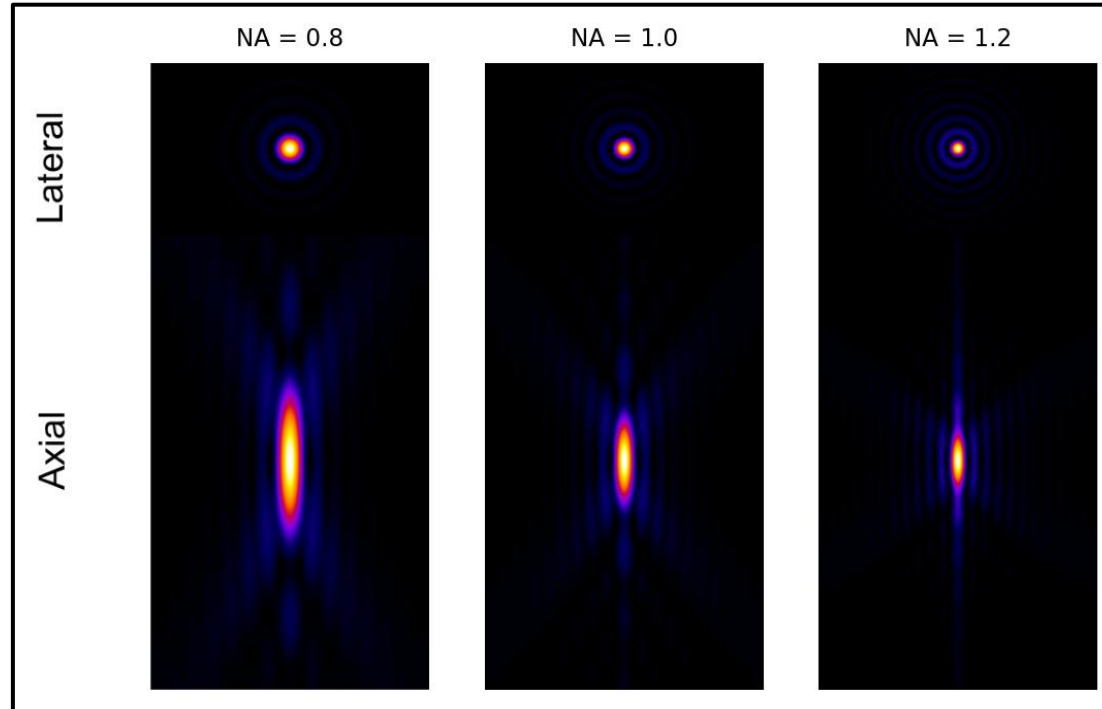
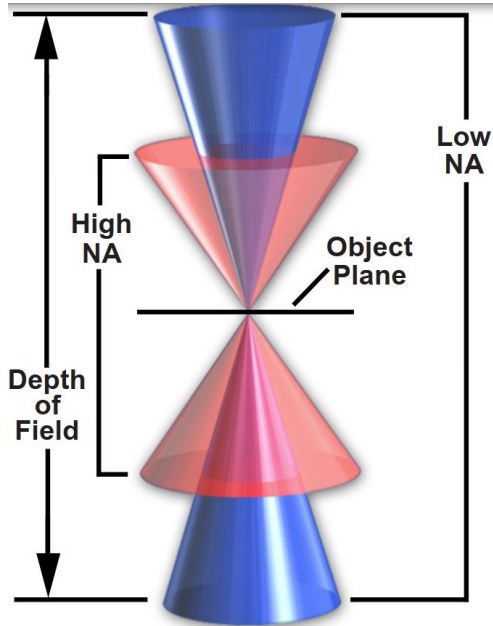
θ : is the half-angle of the maximum cone of light that can enter or exit the lens

The numerical aperture of a microscope objective is a measure of its ability to **gather light** and **resolve** fine specimen detail at a fixed object distance.



<https://www.teledynevisionsolutions.com/learn/learning-center/scientific-imaging/resolution-and-numerical-aperture/>

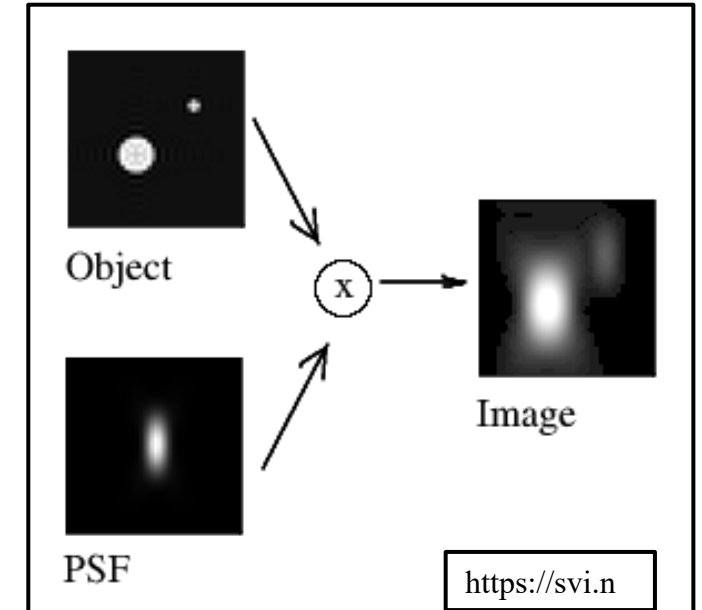
Image formation, PSF, and Resolution



<https://bioimagebook.github.io/>

$$\text{Abbe Lateral Res} \sim \frac{\lambda}{2 n \sin \alpha} = \frac{\lambda}{2 NA}$$

$$\text{Abbe Axial Res} \sim \frac{2\lambda}{(NA)^2}$$



$$g = h * f$$

The image (g) = the convolution of the object (f) and the PSF (h)

PSF: Point Spread Function (how a point-like object appears)

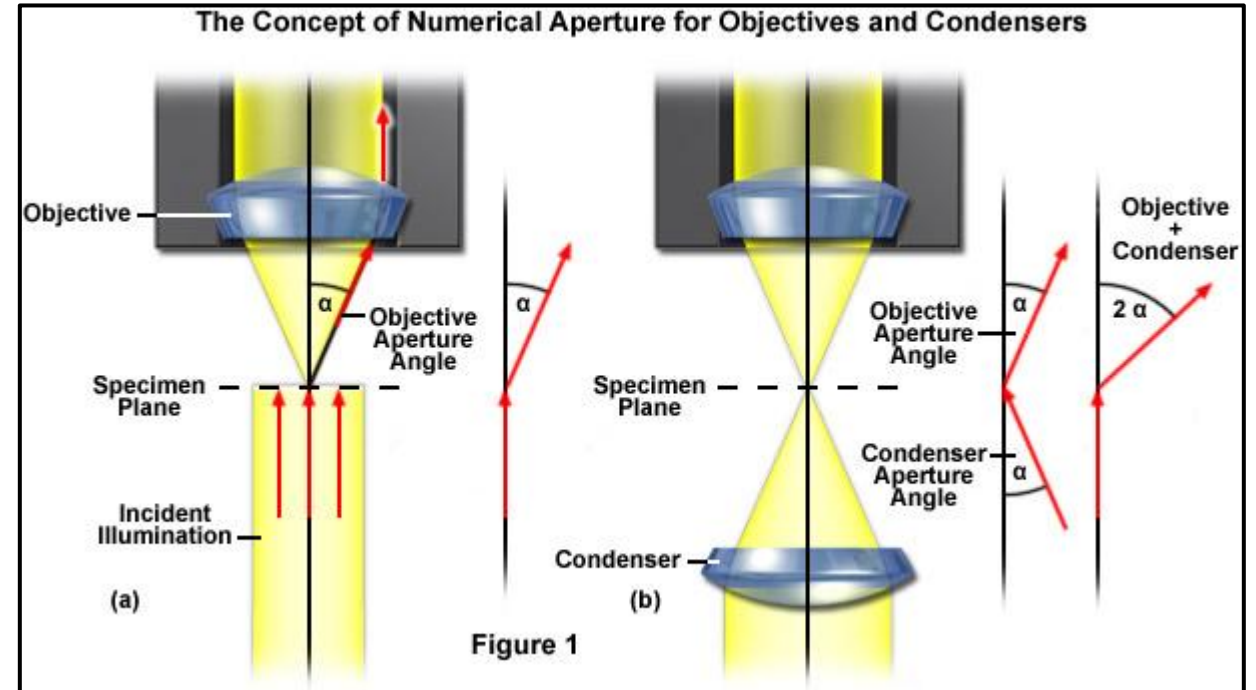
Resolution and NA dependence

$$\text{Lateral Res} \sim \frac{\lambda}{2 n \sin \alpha} = \frac{\lambda}{2 NA}$$

$$\text{Axial Res} \sim \frac{2\lambda}{(NA)^2}$$

If $NA_{cond} \leq NA_{obj}$:

$$\text{Lateral Res} \sim \frac{1.22 \lambda}{NA_{obj} + NA_{cond}} \text{ (Abbe formula)}$$

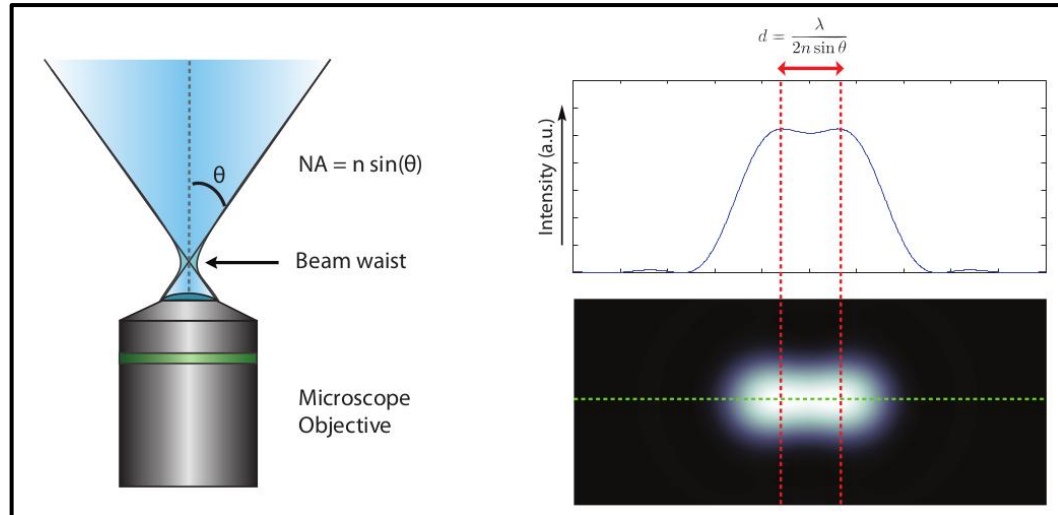


<https://zeiss-campus.magnet.fsu.edu/>

In epi FL microscopes the objective acts as the condenser:

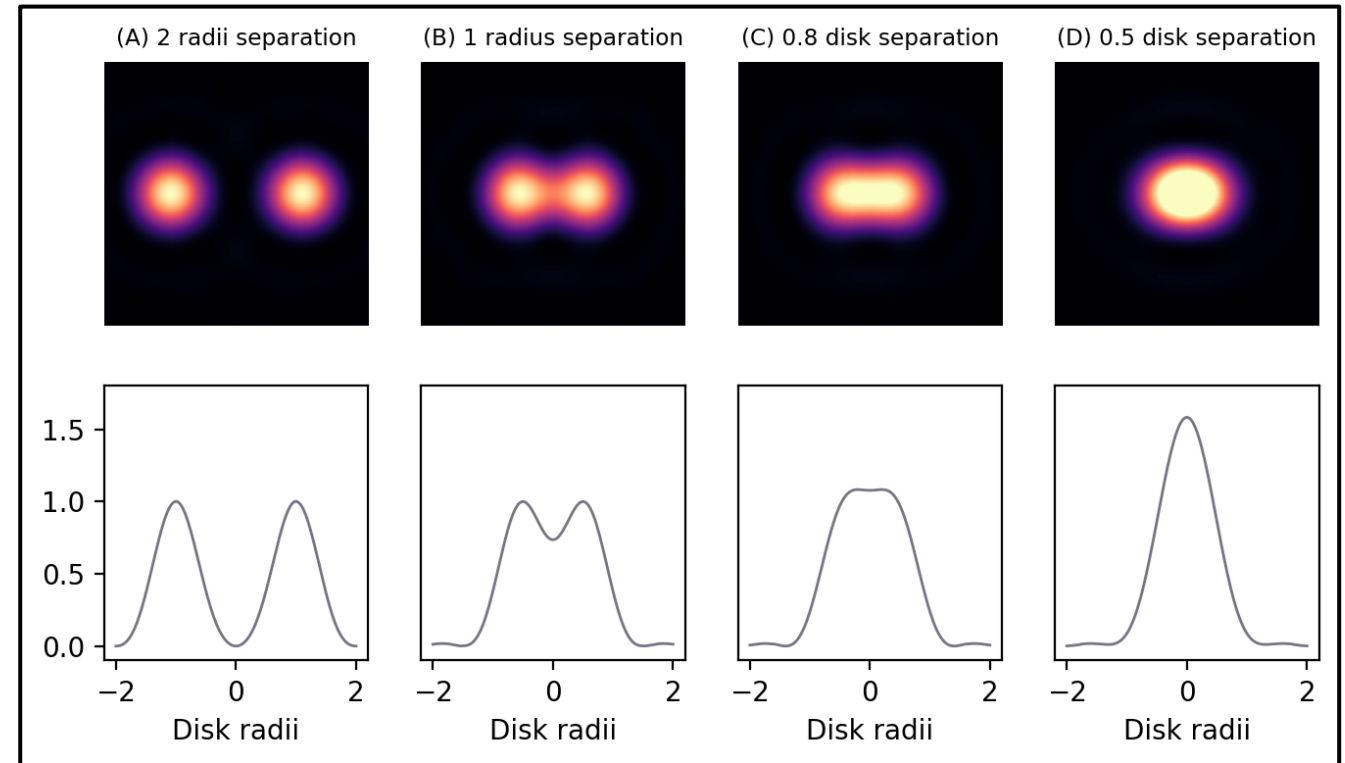
Lateral resolution: only objective NA

Resolution Limit Imposed by **Wave Nature** of Light



$$\text{Rayleigh Lateral Res } n \sin \theta = \frac{\lambda}{2d}$$

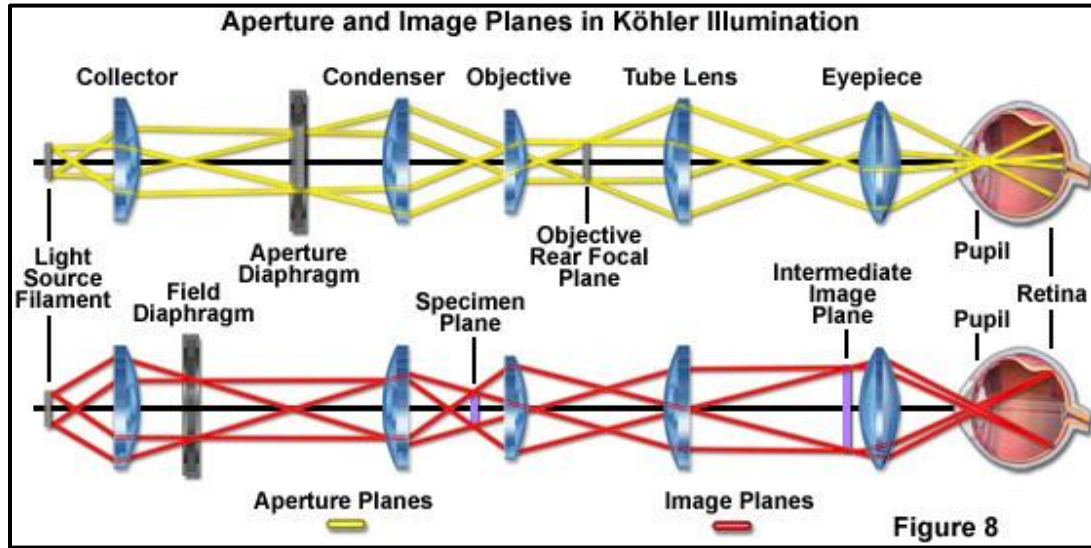
$$d = 0.61 \frac{\lambda}{NA}$$



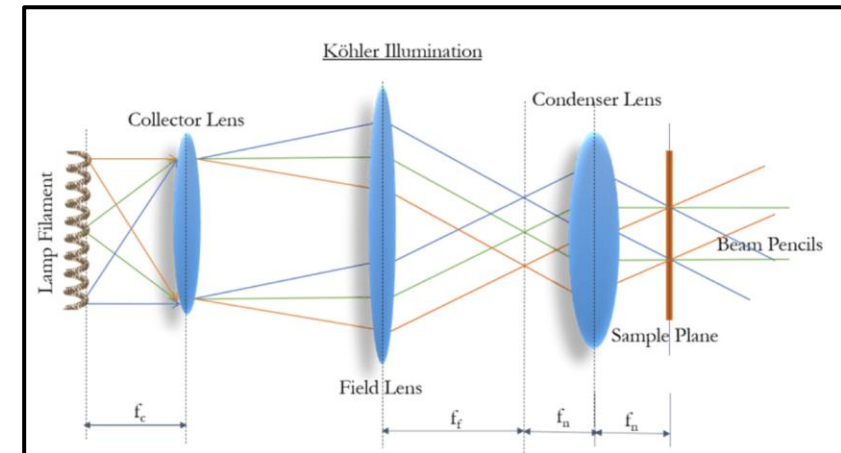
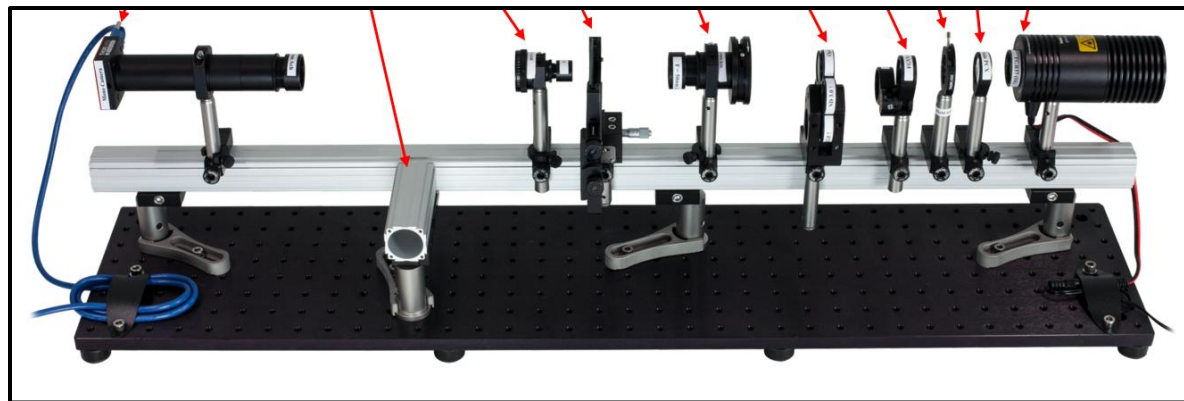
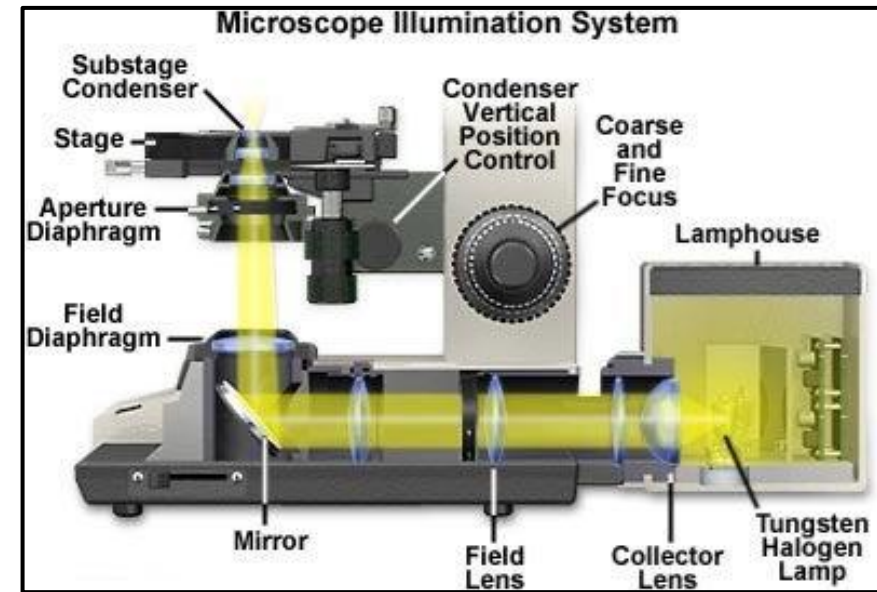
<https://bioimagebook.github.io/>

The Rayleigh criterion : the minimum resolvable detail.
 “The first diffraction minimum of the image of one source point coincides with the maximum of another.”

Uniform illumination using several lenses



<https://zeiss-campus.magnet.fsu.edu/>



www.teledynevisionsolutions.com/

Microscope main components

Illumination Sources



Optical Components



Detectors



Data Acquisition Components



Microscope main components – Illumination sources

Lamps



Broad spectral excitation

LEDs



Cheap, Long-lasting, Poor spectral purity, Hard to focus into fibers, Portable systems

Laser Diodes

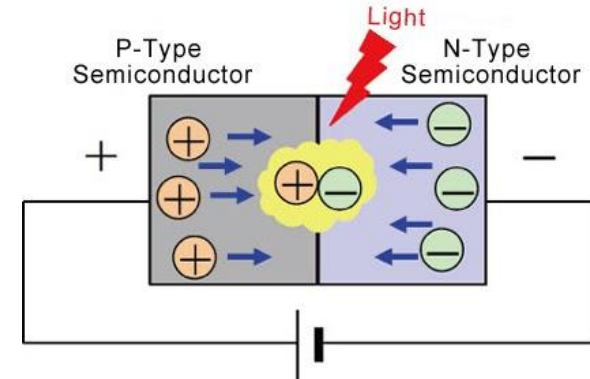


High-power, Better coherence, Stable, Easy to couple w/ fibers, Delicate – easy to burn down, More expensive

Laser Systems



Desired bandwidth, wavelength, stability, frequency, high coherence, Most expensive



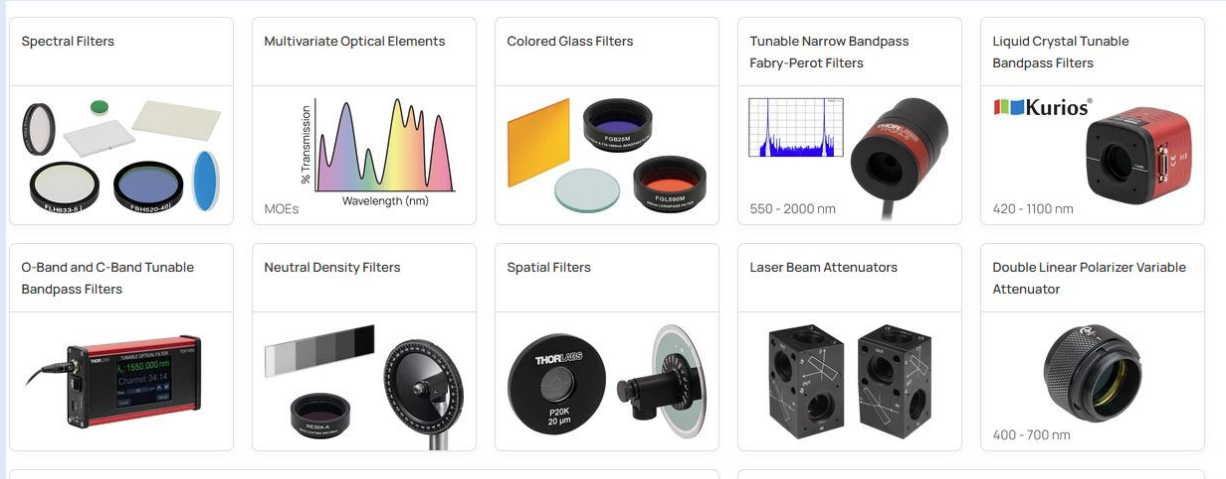
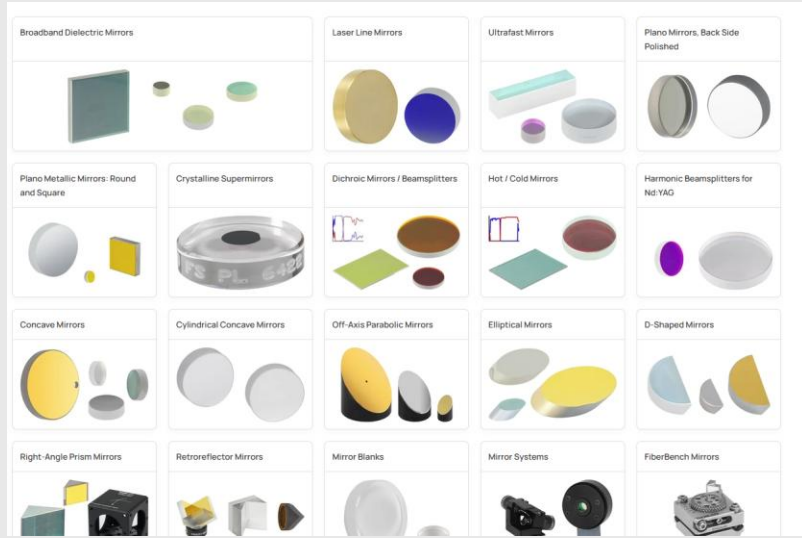
Lowest coherence



Highest coherence

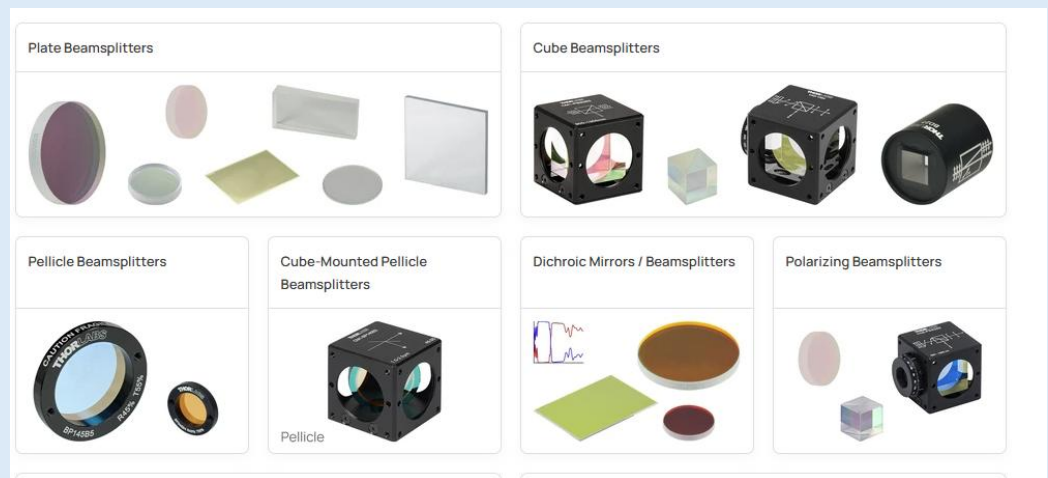
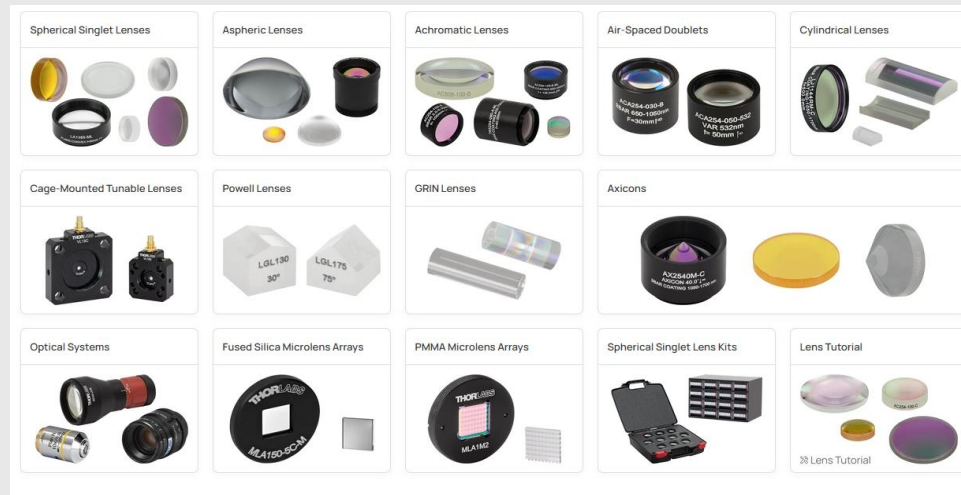
Microscope main components - Optics

Mirrors:
Broadband dielectric,
gold,
cylindrical,
Concave,



Filters: Intensity (ND), bandpass, long/short pass, polarization, ...

Lenses:
Aspheric,
Achromatic,
Convex,
Concave,
Doublet,
Powell,
Cylindrical,
...

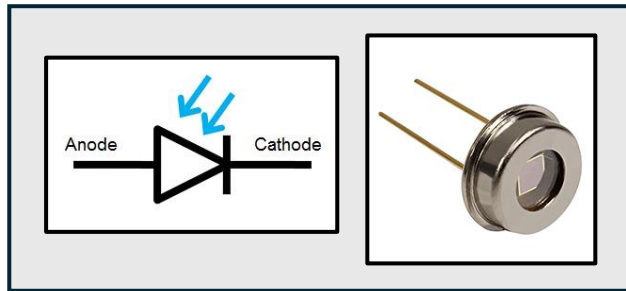


Beamsplitters: X/Y (50/50), Dichromatic, Polarizing,...

Microscope main components - Detectors

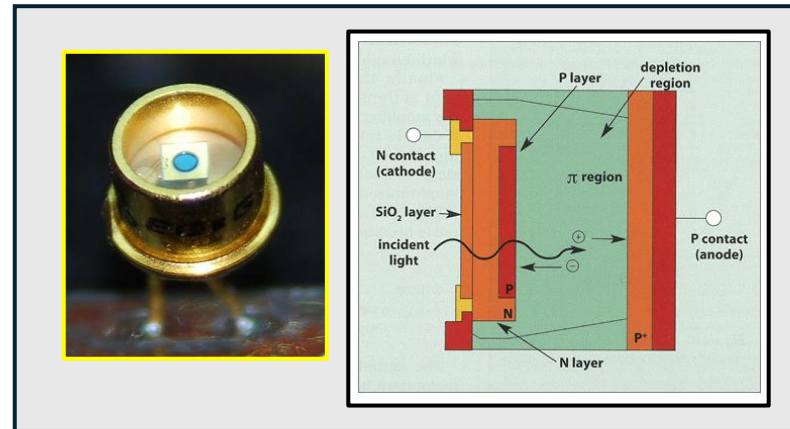
Photodiodes

(PN junction diode in reverse bias)
cheap, high speed, moderate sensitivity



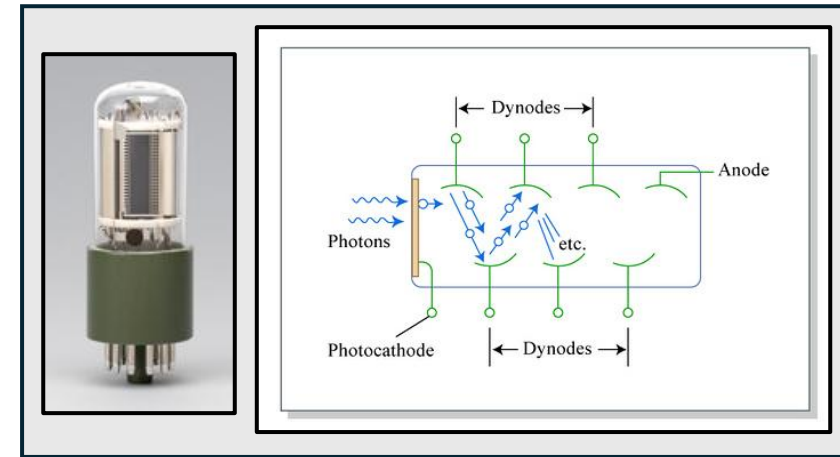
Avalanche Photo Diodes (APD)

high gain/sensitivity, higher cost,
more delicate



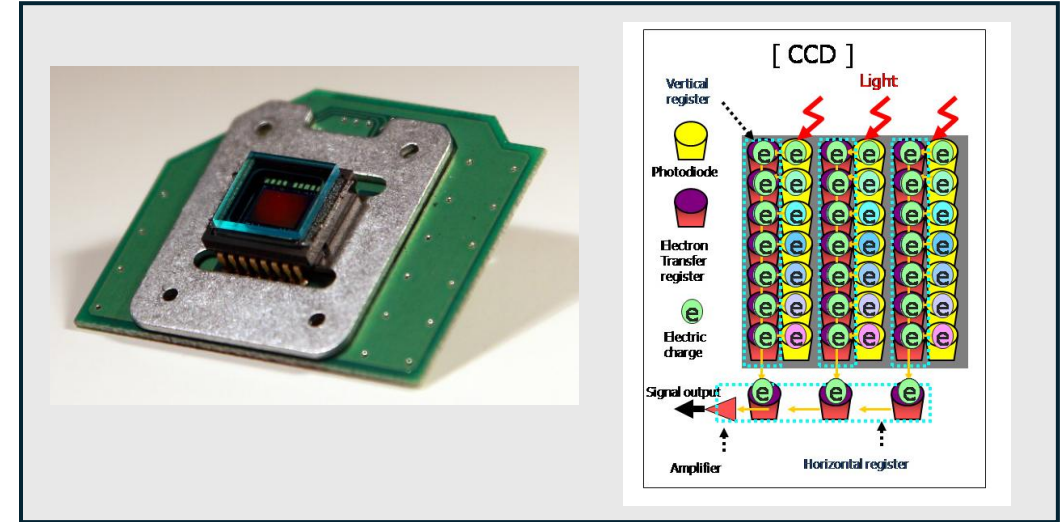
Photomultiplier tubes (PMT)

very high gain/sensitivity,
require high voltage,
prone to damage,
limited near-IR reach (< 850 nm)



Charge coupled devices (CCD)

- Analog
- Linked capacitors transfer charges
- Cheap

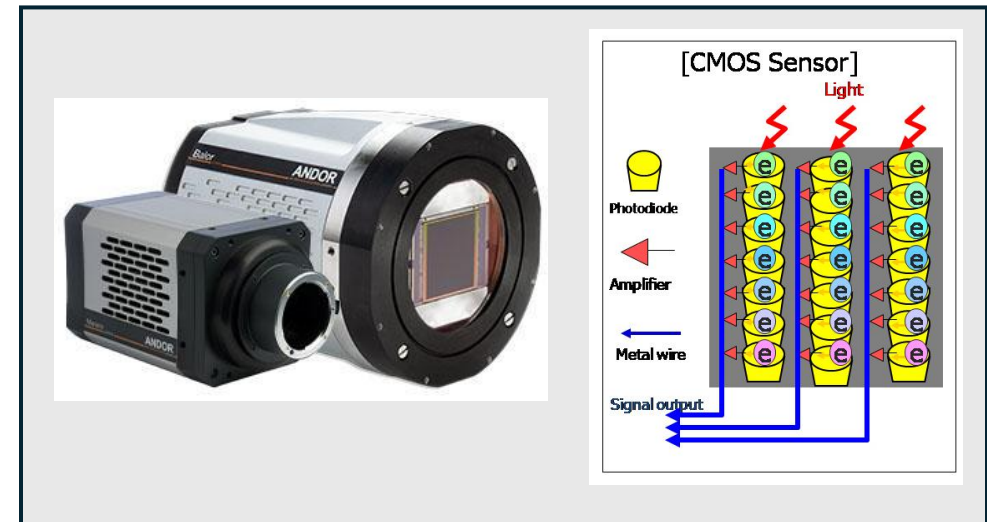


Complementary metal-oxide-semiconductor (CMOS)

- Digital
- High speed
- Low sensitivity

sCMOS (Scientific CMOS)

- Very low noise



Microscope main components - DAQ components

Analog to Digital Card (Digitizer)



- Converts the analog signal pulses to digital ones
- Transfers data ...

Camera (Detector array) Frame Grabber



- Converts the signal pulses from camera (detector array) to digital ones
- Transfers data ...

High Speed Data Storage drive



- Up to several GB/s data transfer speed

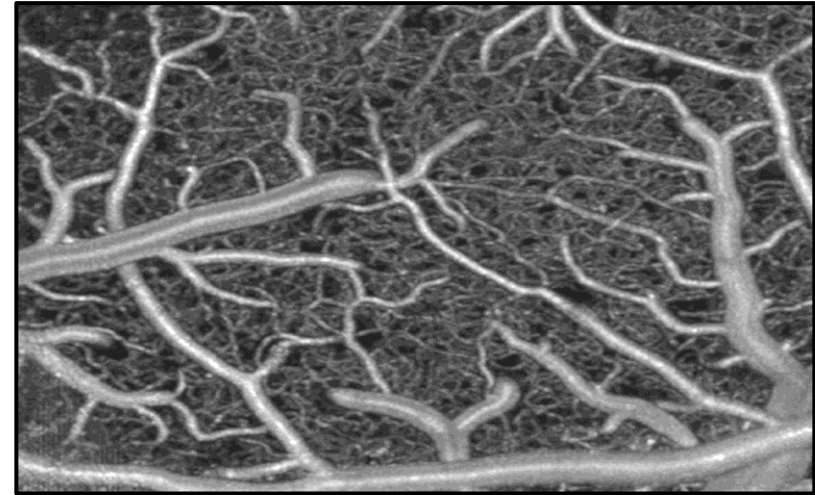
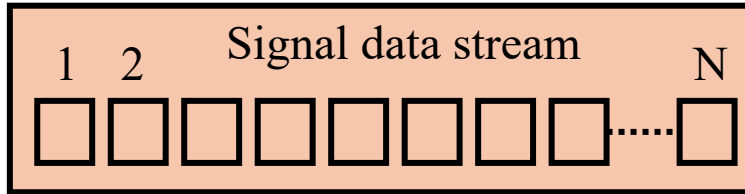
Microscope main components - DAQ components

Multifunction I/O Modules, BNC cables, fibers, etc.

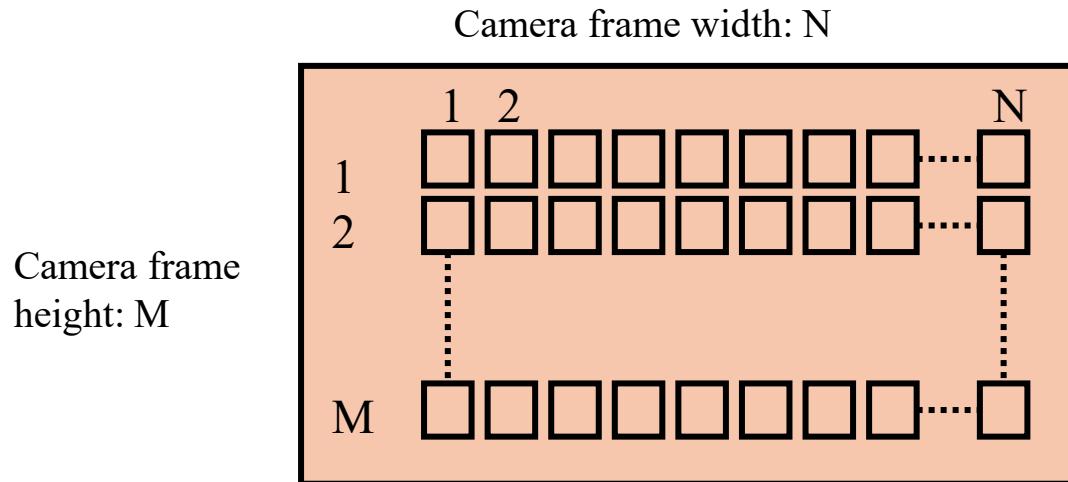


Software (Acquisition & Processing)

Single detector



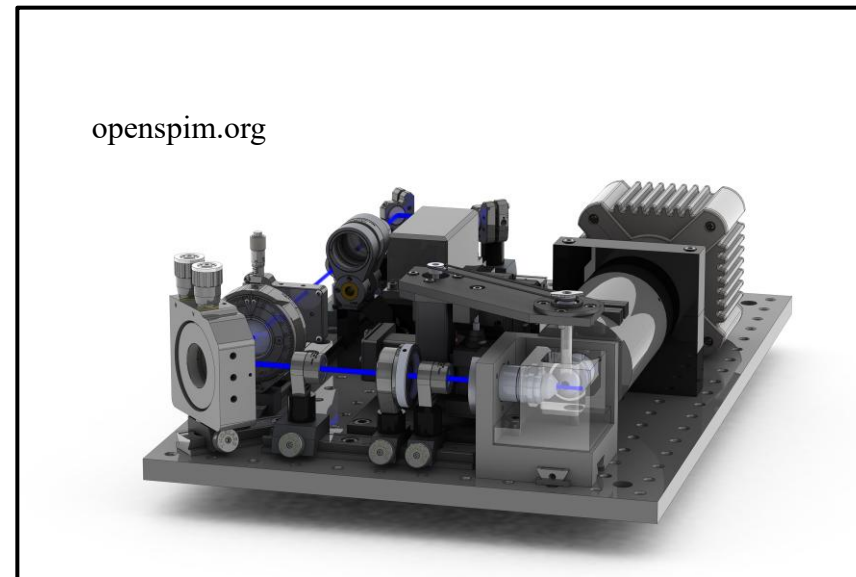
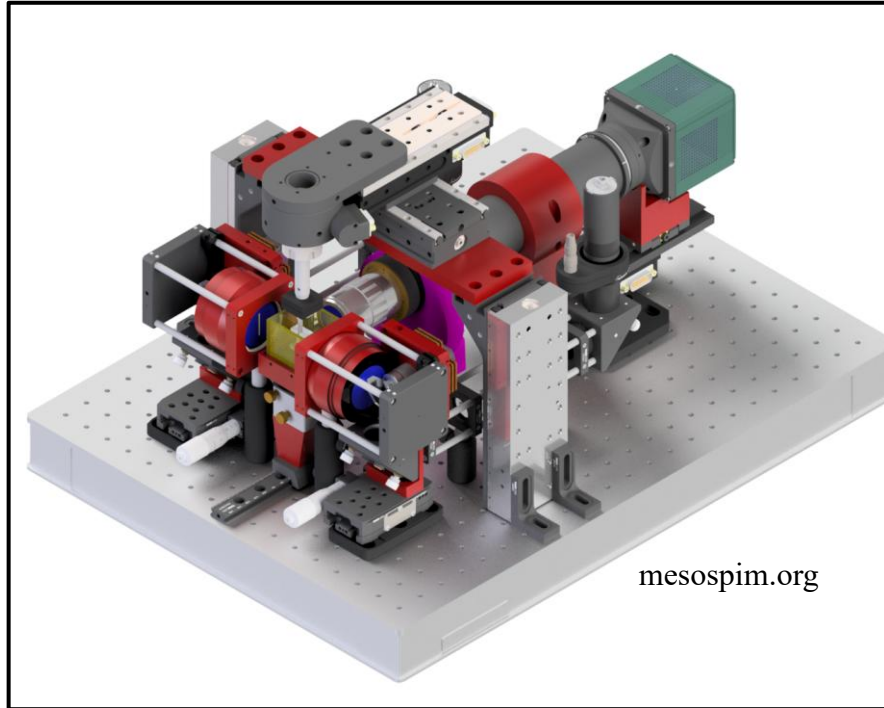
Detector array



Processing procedure could be composed of: Averaging, filtering/Noise removing methods, deconvolution, etc.

(Explained in second session of the course)

Examples of noncommercial microscopes



Thanks

Bio Imaging Resource Center team

Alison North,
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